

(19)



Europäisches Patentamt

European Patent Office

Office européen des brevets



(11)

EP 0 708 331 B1

(12)

EUROPEAN PATENT SPECIFICATION

(45) Date of publication and mention
of the grant of the patent:
24.03.2004 Bulletin 2004/13

(51) Int Cl.7: **G01N 27/447**

(21) Application number: **95116515.8**

(22) Date of filing: **19.10.1995**

(54) Fully integrated miniaturized planar liquid sample handling and analysis device

Miniaturisierte vollintegrierte planare Flüssigkeitsprobenhandhabungs- und -analysevorrichtung

Dispositif miniaturisé et complètement intégré pour l'analyse et manoeuvre des échantillons liquides

(84) Designated Contracting States:
CH DE GB LI SE

(30) Priority: **19.10.1994 US 326111**
07.06.1995 US 486024

(43) Date of publication of application:
24.04.1996 Bulletin 1996/17

(73) Proprietor: **Agilent Technologies, Inc. (a Delaware corporation)**
Palo Alto, CA 94303 (US)

(72) Inventors:
• **Witt, Klaus E.**
D-75210 Keltern (DE)
• **Kaltenbach, Patrick**
D-76476 Bischweier (DE)
• **Bek, Fritz**
D-76337 Waldbronn (DE)

• **Swedberg, Sally A.**
Los Altos, CA 94022 (US)
• **Mittelstadt, Laurie S.**
Belmont, CA 94002 (US)

(74) Representative: **Schoppe, Fritz, Dipl.-Ing.**
Schoppe, Zimmermann, Stöckeler & Zinkler
Patentanwälte
Postfach 246
82043 Pullach bei München (DE)

(56) References cited:
WO-A-96/03206 **US-A- 4 891 120**
US-A- 4 908 112 **US-A- 5 132 012**

• **ROBERT A.MEYERS, EDITOR:**
"ENCYCLOPEDIA OF PHYSICAL SCIENCE AND TECHNOLOGY", 1987, ACADEMIC PRESS, INC., ORLANDO, FLORIDA

Note: Within nine months from the publication of the mention of the grant of the European patent, any person may give notice to the European Patent Office of opposition to the European patent granted. Notice of opposition shall be filed in a written reasoned statement. It shall not be deemed to have been filed until the opposition fee has been paid. (Art. 99(1) European Patent Convention).

EP 0 708 331 B1

Description

Technical Field

[0001] The present invention relates generally to miniaturized planar column technology for liquid phase analysis. More particularly the invention relates to a miniaturized total analysis system (μ -TAS) fabricated in novel separation support media using laser ablation techniques. The μ -TAS disclosed herein finds use in the liquid phase analysis of either small and/or macromolecular solutes.

Background

[0002] In sample analysis instrumentation, and especially in separation systems such as liquid chromatography and capillary electrophoresis systems, smaller dimensions will generally result in improved performance characteristics and at the same time result in reduced production and analysis costs. In this regard, miniaturized separation systems provide more effective system design, result in lower overhead due to decreased instrumentation sizing and additionally enable increased speed of analysis, decreased sample and solvent consumption and the possibility of increased detection efficiency.

[0003] Accordingly, several approaches towards miniaturization for liquid phase analysis have developed in the art; the conventional approach using drawn fused-silica capillary, and an evolving approach using silicon micromachining. What is currently thought of as conventional in miniaturization technology is generally any step toward reduction in size of the analysis system.

[0004] In conventional miniaturized technology the instrumentation has not been reduced in size; rather, it is the separation compartment size which has been significantly reduced. As an example, micro-column liquid chromatography (μ LC) has been described wherein columns with diameters of 100-200 μ m are employed as compared to prior column diameters of around 4.6 mm.

[0005] Another approach towards miniaturization has been the use of capillary electrophoresis (CE) which entails a separation technique carried out in capillaries 25-100 μ m in diameter. CE has been demonstrated to be useful as a method for the separation of small solutes. *J. Chromatogr.* 218:209 (1981); *Analytical Chemistry* 53:1298 (1981). In contrast, polyacrylamide gel electrophoresis was originally carried out in tubes 1 mm in diameter. Both of the above described "conventional" miniaturization technologies (pLC and CE) represent a first significant step toward reducing the size of the chemical portion of a liquid phase analytical system. However, even though experimentation with such conventional miniaturized devices has helped to verify the advantages of miniaturization in principal, there nevertheless remain several major problems inherent in those technologies.

[0006] For example, there remains substantial detection limitations in conventional capillary electrophoresis technology. For example, in CE, optical detection is generally performed on-column by a single-pass detection technique wherein electromagnetic energy is passed through the sample, the light beam travelling normal to the capillary axis and crossing the capillary only a single time. Accordingly, in conventional CE systems, the detection path length is inherently limited by the diameter of the capillary.

[0007] Given Beer's law, which relates absorbance to the path length through the following relationship:

$$A = \epsilon \cdot b \cdot C$$

where:

A = the absorbance

ϵ = the molar absorptivity, (l/m^*cm)

b = path length (cm)

C = concentration (m/l)

it can be readily understood that the absorbance (A) of a sample in a 25 μ m capillary would be a factor of 400x less than it would be in a conventional 1 cm path length cell as typically used in UV/Vis spectroscopy.

[0008] In light of this significant detection limitation, there have been a number of attempts employed in the prior art to extend detection path lengths, and hence the sensitivity of the analysis in CE systems. In U.S. Patent No. 5,061,361 to Gordon, there has been described an approach entailing micro-manipulation of the capillary flow-cell to form a bubble at the point of detection. In U.S. Patent No. 5,141,548 to Chervet, the use of a Z-shaped configuration in the capillary, with detection performed across the extended portion of the Z has been described. Yet another approach has sought to increase the detection path length by detecting along the major axis of the capillary (axial-beam detection). Xi et al., *Analytical Chemistry* 62:1580 (1990).

[0009] In U.S. Patent No. 5,273,633 to Wang, a further approach to increased detection path lengths in CE has been described where a reflecting surface exterior of the capillary is provided, the subject system further including an incident window and an exit window downstream of the incident window. Under Wang, light entering the incident window passes through a section of the capillary by multiple internal reflections before passing through the exit window where it is detected, the subject multiple internal reflections yielding an effective increase in path length. While each of the aforementioned approaches has addressed the issue of extending the path length, each approach is limited in that it entails engineering the capillary after-the-fact or otherwise increasing the cost of the analysis.

[0010] A second major drawback in the current approach to miniaturization involves the chemical activity

and chemical instability of silicon dioxide (SiO_2) substrates, such as silica, quartz or glass, which are commonly used in both CE and μLC systems. More particularly, silicon dioxide substrates are characterized as high energy surfaces and strongly adsorb many compounds, most notably bases. The use of silicon dioxide materials in separation systems is further restricted due to the chemical instability of those substrates, as the dissolution of SiO_2 materials increases in basic conditions (at pHs greater than 7.0).

[0011] To avoid the problems arising from the inherent chemical activity of silicon dioxide materials, prior separation systems have attempted chemical modifications to the inner silica surface of capillary walls. In general, such post-formation modifications are difficult as they require the provision of an interfacial layer to bond a desired surface treatment to the capillary surface, using, for example, silylating agents to create Si-O-Si-C bonds. Although such modifications may decrease the irreversible adsorption of solute molecules by the capillary surfaces, these systems still suffer from the chemical instability of Si-O-Si bonds at pHs above 7.0. Accordingly, chemical instability in SiO_2 materials remains a major problem.

[0012] However, despite the recognized shortcomings with the chemistry of SiO_2 substrates, those materials are still used in separation systems due to their desirable optical properties. In this regard, potential substitute materials which exhibit superior chemical properties compared to silicon dioxide materials are generally limited in that they are also highly adsorbing in the UV region, where detection is important.

[0013] In order to avoid some of the substantial limitations present in conventional μLC and CE techniques, and in order to enable even greater reduction in separation system sizes, there has been a trend towards providing planarized systems having capillary separation microstructures. In this regard, production of miniaturized separation systems involving fabrication of microstructures in silicon by micromachining or microlithographic techniques has been described. See, e.g. Fan et al., *Anal. Chem.* **66**(1):177-184 (1994); Manz et al., *Adv. Chrom.* **33**:1-66 (1993); Harrison et al., *Sens. Actuators*, **B10**(2):107-116 (1993); Manz et al., *Trends Anal. Chem.* **10**(5):144-149 (1991); and Manz et al., *Sensors and Actuators B (Chemical)* **B1**(1-6):249-255 (1990).

[0014] State-of-the-art chemical analysis systems for use in chemical production, environmental analysis, medical diagnostics and basic laboratory analysis must be capable of complete automation. Such a total analysis system (TAS) (Fillipini et al (1991) *J. Biotechnol.* **18**: 153; Garn et al (1989) *Biotechnol. Bioeng.* **34**:423; Tshulena (1988) *Phys. Scr.* **T23**:293; Edmonds (1985) *Trends Anal. Chem.* **4**:220; Stinshoff et al. (1985) *Anal. Chem.* **57**:114R; Guibault (1983) *Anal. Chem. Symp. Ser.* **17**:637; Widmer (1983) *Trends Anal. Chem.* **2**:8) automatically performs functions ranging from introduc-

tion of sample into the system, transport of the sample through the system, sample preparation, separation, purification and detection, including data acquisition and evaluation. Miniaturized total analysis systems have been referred to as " $\mu\text{-TAS}$."

[0015] Recently, sample preparation technologies have been successfully reduced to miniaturized formats. Gas chromatography (Widmer et al. (1984) *Int. J. Environ. Anal. Chem.* **18**:1), high pressure liquid chromatography (Müller et al. (1991) *J. High Resolut. Chromatogr.* **14**:174; Manz et al.. (1990) *Sensors & Actuators B1*:249; Novotny et al., eds. (1985) *Microcolumn Separations: Columns, Instrumentation and Ancillary Techniques* (J. Chromatogr. Library, Vol. 30); Kucera, ed. (1984) *Micro-Column High Performance Liquid Chromatography*, Elsevier, Amsterdam; Scott, ed. (1984) *Small Bore Liquid Chromatography Columns: Their Properties and Uses*, Wiley, NY; Jorgenson et al. (1983) *J. Chromatogr.* **255**:335; Knox et al. (1979) *J. Chromatogr.* **186**:405; Tsuda et al. (1978) *Anal. Chem.* **50**:632) and capillary electrophoresis (Manz et al. (1992) *J. Chromatogr.* **593**:253; Manz et al. *Trends Anal. Chem.* **10**:144; Olefirowicz et al. (1990) *Anal. Chem.* **62**:1872; Second Int'l Symp. High-Perf. Capillary Electrophoresis (1990) *J. Chromatogr.* **516**; Ghowsi et al. (1990) *Anal. Chem.* **62**:2714) have been reduced to miniaturized formats.

[0016] Capillary electrophoresis has been particularly amenable to miniaturization because the separation efficiency is proportional to the applied voltage regardless of the length of the capillary. Harrison et al. (1993) *Science* **261**:895-897. A capillary electrophoresis device using electroosmotic fluid pumping and laser fluorescence detection has been prepared on a planar glass microstructure. Effenhauser et al. (1993) *Anal. Chem.* **65**:2637-2642; Burggraf et al. (1994) *Sensors and Actuators B20*:103-110. In contrast to silicon materials (see, Harrison et al. (1993) *Sensors and Actuators B10*: 107-116), polyimide has a very high breakdown voltage, thereby allowing the use of significantly higher voltages.

[0017] The use of micromachining techniques to fabricate separation systems in silicon provides the practical benefit of enabling mass production of such systems. In this regard, a number of established techniques developed by the microelectronics industry involving micromachining of planar materials, such as silicon, exist and provide a useful and well accepted approach to miniaturization. Examples of the use of such micromachining techniques to produce miniaturized separation devices on silicon or borosilicate glass chips can be found in U.S. Patent No. 5,194,133 to Clark et al.; U.S. Patent No. 5,132,012 to Miura et al.; in U.S. Patent No. 4,908,112 to Pace; and in U.S. Patent No. 4,891,120 to Sethi et al.

[0018] Micromachining silicon substrates to form miniaturized separation systems generally involves a combination of film deposition, photolithography, etching and bonding techniques to fabricate a wide array of

three dimensional structures. Silicon provides a useful substrate in this regard since it exhibits high strength and hardness characteristics and can be micromachined to provide structures having dimensions in the order of a few micrometers.

[0019] Although silicon micromachining has been useful in the fabrication of miniaturized systems on a single surface, there are significant disadvantages to the use of this approach in creating the analysis device portion of a miniaturized separation system.

[0020] Initially, silicon micromachining is not amenable to producing a high degree of alignment between two etched or machined pieces. This has a negative impact on the symmetry and shape of a separation channel formed by micromachining, which in turn may impact separation efficiency. Secondly, sealing of micromachined silicon surfaces is generally carried out using adhesives which may be prone to attack by separation conditions imposed by liquid phase analyses. Furthermore, under oxidizing conditions, a silica surface is formed on the silicon chip substrate. In this regard, silicon micromachining is also fundamentally limited by the chemistry of SiO_2 .

[0021] WO 96/03206 (falling under the provisions of Art. 54(3) EPC) relates to an integral structure for chemical processing, such as high-speed mixing and chemical reacting, which consists of a number of laminae joined together and having inlet and outlet ports connecting a plurality of intersecting channels formed in the respective side surfaces of the laminae. In the illustrated embodiments, each lamina comprises a silicon wafer which has the major planar surface of the wafer in the (100) crystal plane. Channels are formed by an anisotropic edge. Wear resistant coatings, such as metalloid carbides, in the form of thin films, may be optionally deposited on the processed laminae before bonding.

[0022] US-A-4,891,120 relates to a chromatographic separation device having a body of semiconductor material. The body has a longitudinal channel formed in a surface of the body of semiconductor material. The channel may be formed by integrated circuit techniques, such as photolithography and micromachining. Alternatively, the channel may be formed by a micromechanical machining technique, such as electromechanical sawing.

[0023] It is an object of the invention to provide a miniaturized column device for use in liquid phase analysis.

[0024] This object is achieved by a miniaturized column device in accordance with claim 1.

[0025] The present invention is also related to the provision of detection means engineered into a miniaturized planar column device whereby enhanced on-column analysis or detection of components in a liquid sample is enabled. It is further contemplated to provide a column device for liquid phase analysis having detection means designed into the device in significantly compact form as compared to conventional technology. In one particular aspect of the present invention, it is con-

templated to provide optical detection means ablated in a miniaturized planar column device and having a substantially enhanced detection path length.

[0026] It is a further related object of the present invention to provide a device featuring improved means for liquid handling, including sample injection, and to provide a miniaturized column device with means to interface with a variety of external liquid reservoirs. Specifically contemplated herein is a system design which allows a variety of injection methods to be readily adapted to the planar structure, such as pressure injection, hydrodynamic injection or electrokinetic injection.

[0027] In this regard, a miniaturized system according to the present invention is capable of performing complex sample handling, separation, and detection methods with reduced technician manipulation or interaction. Accordingly, the subject invention finds potential application in monitoring and/or analysis of components in industrial chemical, biological, biochemical and medical processes and the like.

[0028] A particular advantage of the present invention is the use of processes other than silicon micromachining techniques or etching techniques to create miniaturized columns in a wide variety of polymeric and ceramic substrates having desirable attributes for an analysis portion of a separation system. More specifically, it is contemplated herein to provide a miniaturized planar column device by ablating component microstructures in a substrate using laser radiation. The miniaturized column device is formed by providing two substantially planar halves having microstructures laser-ablated thereon, which, when the two halves are folded upon each other, define a sample processing compartment featuring enhanced symmetry and axial alignment.

[0029] Use of laser ablation techniques to form miniaturized devices according to the present invention affords several advantages over prior etching and micromachining techniques used to form systems in silicon or silicon dioxide materials. Initially, the capability of applying rigid computerized control over laser ablation processes allows microstructure formation to be executed with great precision, thereby enabling a heightened degree of alignment in structures formed by component parts. The laser ablation process also avoids problems encountered with microlithographic isotropic etching techniques which may undercut masking during etching, giving rise to asymmetrical structures having curved side walls and flat bottoms.

[0030] Laser ablation further enables the creation of microstructures with greatly reduced component size. In this regard, microstructures formed according to the invention are capable of having aspect ratios several orders of magnitude higher than possible using prior etching techniques, thereby providing enhanced sample processing capabilities in such devices. The use of laser-ablation processes to form microstructures in substrates such as polymers increases ease of fabrication and lowers per-unit manufacturing costs in the subject

devices as compared to prior approaches such as micromachining devices in silicon. In this regard, devices formed according to the invention in low-cost polymer substrates have the added feature of being capable of use as substantially disposable miniaturized column units.

[0031] Laser-ablation in planar substrates allows for the formation of microstructures of almost any geometry or shape. This feature not only enables the formation of complex device configurations, but further allows for integration of sample preparation, sample injection, post-column reaction and detection means in a miniaturized total analysis system of greatly reduced overall dimensions.

[0032] The compactness of the analysis portion in a device produced under to the present invention, in conjunction with the feature that integral functions such as injection, sample handling and detection may be specifically engineered into the subject device to provide a μ -TAS device, further allows for integrated design of system hardware to achieve a greatly reduced system footprint.

[0033] By the present invention, inherent weaknesses existing in prior approaches to liquid phase separation device miniaturization, and problems in using silicon micromachining techniques to form miniaturized column devices have been addressed. Accordingly, the present invention discloses a miniaturized total analysis system capable of performing a variety of liquid phase analyses on a wide array of liquid samples.

Brief Description of the Figures

[0034]

Figure 1 is an exploded view of a miniaturized column device.

Figure 2 is a plan view of the interior surface of the miniaturized column device of Figure 1.

Figure 3 is a plan view of the exterior surface of the device of Figure 1.

Figure 4 is a cross-sectional side view of the miniaturized column device of Figure 1, taken along lines IV-IV and showing formation of a sample processing compartment.

Figure 5 is an exploded view of a miniaturized column device including optical detection means.

Figure 6 is a cross-sectional axial view of the intersection of the sample processing compartment and the optical detection means in the miniaturized column device of Figure 5.

Figure 7A is an exploded view of a first side of a miniaturized column device having microchannels formed on two opposing planar surfaces of a support substrate.

Figure 7B is an exploded view of a second side of the column device of Figure 7A.

Figure 8A is a pictorial representation of a first side

of a miniaturized column device of Figure 7A which is constructed from a single flexible substrate.

Figure 8B is a pictorial representation of a second side of the column device of Figure 8A.

Figure 9 is a cross-sectional trans-axial view of the extended optical detection path length in the miniaturized column of Figure 8 taken along lines IX-IX. Figure 10 is plan view of a miniaturized column device constructed according to the invention having first and second component halves.

Figure 11 is a pictorial representation of the column device of Figure 10 showing the folding alignment of the component halves to form a single device.

Figure 12 is a cross-sectional axial view of the sample processing compartment formed by the alignment of the component halves in the device of Figure 10.

Figure 13 is a plan view of a further preferred embodiment of the present invention having optional micro-alignment means on first and second component halves.

Figure 14 is a pictorial representation of the column device of Figure 13 showing the micro-alignment of the component halves.

Figure 15 is a diagram of an exemplary μ -TAS.

Figure 16 is an illustration of a μ -TAS having a laser-ablated reservoir compartment as an integral microstructure on the substrate.

Figure 17A is a cross-section of the μ -TAS of Figure 15 showing laser-ablated microstructures for communicating a sample droplet formed by a pressure pulse to a post-column sample collection device having laser-ablated sample droplet receiving microwells. Figure 17B is a cross-section of the μ -TAS of Figure 15 showing laser-ablated microstructures for communicating a sample droplet formed by a generating steam bubbles to a post-column sample collection device having laser-ablated sample droplet receiving microwells and a cover plate. Figure 17C is a cross-section of the μ -TAS of Figure 15 showing laser-ablated microstructures for communicating a sample droplet formed by a generating steam bubbles in a makeup fluid stream to a post-column sample collection device having a sample droplet receiving bibulous sheet means.

Figure 18A is a pictorial representation of the μ -TAS of Figure 15 interfaced with a post-column collection device having sample droplet receiving wells.

Figure 18B is a pictorial representation of the μ -TAS of

Figure 15 interfaced with a post-column collection device having sample droplet receiving wells and a cover plate.

Detailed Description of the Invention

[0035] Before the invention is described in detail, it is to be understood that this invention is not limited to the

particular component parts of the devices described or process steps of the methods described as such devices and methods may vary. It is also to be understood that the terminology used herein is for purposes of describing particular embodiments only, and is not intended to be limiting.

[0036] In this specification and in the claims which follow, reference will be made to a number of terms which shall be defined to have the following meanings:

[0037] The term "substrate" is used herein to refer to any material which is UV-adsorbing, capable of being laser-ablated and which is not silicon or a silicon dioxide material such as quartz, fused silica or glass (borosilicates). Accordingly, miniaturized column devices are formed herein using suitable substrates, such as laser ablatable polymers (including polyimides and the like) and ceramics (including aluminum oxides and the like). Further, miniaturized column devices are formed herein using composite substrates such as laminates. A "laminate" refers to a composite material formed from several different bonded layers of same or different materials. One particularly preferred composite substrate comprises a polyimide laminate formed from a first layer of polyimide, such as Kapton® (DuPont; Wilmington, Delaware), that has been co-extruded with a second, thin layer of a thermal adhesive form of polyimide known as KJ® (DuPont). This thermoplastic adhesive can be applied to one or both sides of the first polyimide layer, thereby providing a means for producing a laminate of desired thickness.

[0038] The term "sample handling region" refers to a portion of a microchannel, or to a portion of a "sample processing compartment" that is formed upon enclosure of the microchannel by a substrate in which a mirror image of the microchannel has been laser ablated as described in detail below, that includes a "sample flow component" or a "sample treatment component." By the term "sample flow component" is intended a portion of the sample processing compartment that interconnects sample treatment components.

[0039] A "sample treatment component" is a portion of the sample processing compartment in which particular sample preparation chemistries are done. In particular, an analyte of interest is generally obtained in a matrix containing other species which may potentially interfere with the detection and analysis of the analyte. Accordingly, a sample treatment component is a portion of the sample processing compartment in which analyte separation from the matrix is effected. Examples of functions which may be served by the sample treatment component include chromatographic separations, electrophoretic separations, electrochromatographic separations, and the like.

[0040] As used herein, the term "detection means" refers to any means, structure or configuration which allows one to interrogate a sample within the sample processing compartment using analytical detection techniques well known in the art. Thus, a detection

means includes one or more apertures, elongated apertures or grooves which communicate with the sample processing compartment and allow an external detection apparatus or device to be interfaced with the sample processing compartment to detect an analyte passing through the compartment.

[0041] Changes in the electrochemical properties of a liquid sample passing through the sample processing compartment can be detected using detection means which physically contact the sample passing through the sample processing compartment. In one embodiment, an electrode may be placed within, or butt-coupled to a detection means such as an aperture or a groove, thereby enabling the electrode to directly contact the sample stream. By arranging two dissimilar electrodes (which are connected through an external conducting circuit) opposite each other relative to the sample processing compartment, an electric field can be generated in the sample processing compartment--transverse to the direction of sample flow--thereby providing a ready means of electrochemical detection of analytes passing through the compartment.

[0042] Changes in the electrical properties of a liquid sample passing through the sample processing compartment can be detected using detection means which do not physically contact the sample passing through the sample processing compartment. Thus, "changes in the electrical properties" of a sample passing through the sample processing compartment refers to detectable changes in the conductivity, permittivity, or both of a particular sample due to the presence of an analyte in the sample. The "conductivity" of a sample refers to the ratio of the electric current density to the electric field in that sample. The "permittivity" of a sample refers to the dielectric constant of a sample multiplied by the permittivity of empty space, where the permittivity of empty space (ϵ_0) is a constant appearing in coulomb's law having the value of 1 in centimeter-gram-second electrostatic units.

[0043] Changes in the electrical properties of a sample passing through a sample processing compartment are measured herein by detection of the impedance of the liquid sample. The "impedance" or "electrical impedance" of a circuit refers to the total opposition that the circuit presents to an alternating current ("AC"), equal to the complex ratio of the voltage to the current in complex notation. Thus, the magnitude of the total opposition that a circuit presents to an alternating current is equal to the ratio of the maximum voltage in an AC circuit to the maximum current. An "electrical impedance meter" refers to an instrument which measures the complex ratio of voltage to current in a given circuit at a given frequency.

[0044] A plurality of electrical "communication paths" capable of carrying and/or transmitting electric current can be arranged adjacent to the sample processing compartment such that the communication paths, in combination, form a circuit. As used herein, a commu-

nication path includes any conductive material which is capable of transmitting or receiving an AC signal. A particularly preferred conductive material is copper. Thus, in one embodiment, a plurality of communication paths forming an antenna circuit (e.g., a pair of copper antennae) are arranged adjacent to the sample processing compartment whereby a circuit is formed capable of passing an oscillating voltage through the sample processing compartment which is sensitive to changes in the impedance of a liquid sample flowing there-through. An "antenna" refers to a device capable of radiating and/or receiving radio waves such as an alternating current (AC) signal. An "antenna circuit" intends a complete electrical circuit which includes an antenna. An "antenna coil" refers to a coil through which antenna current (e.g., an AC signal) flows.

[0045] Further, by the arrangement of two detection means opposite each other relative to the sample processing compartment, a "detection path" is conveniently formed, thereby allowing detection of analytes passing through the sample processing compartment using detection techniques well known in the art.

[0046] An "optical detection path" refers to a configuration or arrangement of detection means to form a path whereby radiation, such as a ray of light, is able to travel from an external source to a means for receiving radiation--wherein the radiation traverses the sample processing compartment and can be influenced by the sample or separated analytes in the sample flowing through the sample processing compartment. An optical detection path is generally formed according to the invention by positioning a pair of detection means directly opposite each other relative to the sample processing compartment. In this configuration, analytes passing through the sample processing compartment can be detected via transmission of radiation orthogonal to the major axis of the sample processing compartment (and, accordingly, orthogonal to the direction of electro-osmotic flow in an electrophoretic separation). A variety of external optical detection techniques can be readily interfaced with the sample processing compartment using an optical detection path including, but not limited to, UV/Vis, Near IR, fluorescence, refractive index (RI) and Raman techniques.

[0047] As used herein, the term "transparent" refers to the ability of a substance to transmit light of different wavelengths, which ability may be measured in a particular substance as the percent of radiation which penetrates a distance of 1 meter. Thus, according to the invention, a "transparent sheet" is defined as a sheet of a substance which is transmissive to specific types of radiation or particles of interest. Transparent sheets which are particularly employed in the invention in the context of optical detection configurations are formed from materials such as, but not limited to, quartz, sapphire, diamond and fused silica.

[0048] In the context of UV-visible absorption detection of sample analytes herein, the terms "path length,"

or "optical path length" refer to an optical path length "b" derived from Beer's law, which states that $A = \log(I_0/I_t) = \epsilon \cdot b \cdot C$, wherein A is the absorbance, I_0 is the light intensity measured in the absence of the analyte, I_t is the light intensity transmitted through the analyte, ϵ is the molar extinction coefficient of the sample ($l/m \cdot cm$), C is the analyte concentration (m/l), and b is the optical path length (cm). Thus, in a detection configuration wherein UV-Vis absorption of a sample analyte is measured via an optical detection path by passing light through the sample processing compartment along a path perpendicular to the sample processing compartment major axis, the path length (b) of the measurement is substantially defined by the dimensions of the sample processing compartment.

[0049] A "detection intersection" refers to a configuration wherein a plurality of detection means that communicate with the sample processing compartment converge at a particular location in the sample processing compartment. In this manner, a number of detection techniques can be simultaneously performed on a sample or separated analyte at the detection intersection. According to the invention, a detection intersection is formed when a plurality of detection paths cross, or when a detection means such as an aperture communicates with the sample processing compartment at substantially the same point as a detection path. The sample, or a separated analyte, can thus be interrogated using a combination of UV/Vis and fluorescence techniques, optical and electrochemical techniques, optical and electrical techniques, or like combinations to provide highly sensitive detection information. See, e.g., Beckers et al. (1988) *J. Chromatogr.* 452:591-600; and U.S. Patent No. 4,927,265, to Brownlee.

[0050] As used herein, a "lightguide means" refers to a substantially long, thin thread of a transparent substance which can be used to transmit light. Lightguide means useful in the practice of the invention include optical fibers, integrated lens configurations and the like. In particularly preferred embodiments, optical fibers are interfaced with detection means to enable optical detection techniques known in the art. The terms "optical fiber," "fiber optic waveguide" or "optical fiber means" are used herein to refer to a single optical fiber or a bundle of optical fibers, optionally encased in a protective cladding material. Examples of suitable optical fiber substrate materials include glass, plastic, glass/glass composite and glass/plastic composite fibers. A critical characteristic of optical fibers is attenuation of an optical signal. Further, a chemical sensor can be incorporated into a fiber optic waveguide in a manner such that the chemical sensor will interact with the liquid sample analyte. Structures, properties, functions and operational details of such fiber optic chemical sensors can be found in United States Patent No. 4,577,109 to Hirschfeld, U.S. Patent No. 4,785,814 to Kane, and U.S. Patent No. 4,842,783 to Blaylock.

[0051] The use of laser ablation techniques in the

practice of the invention allows for a high degree of precision in the alignment of micro-scale components and structures, which alignment has either been difficult or not possible in prior silicon or glass substrate-based devices. Thus, the term "microalignment" as used herein refers to the precise and accurate alignment of laser-ablated features, including the enhanced alignment of complementary microchannels or microcompartments with each other, inlet and/or outlet ports with microchannels or separation compartments, detection means with microchannels or separation compartments, detection means with other detection means, and the like.

[0052] The term "microalignment means" is defined herein to refer to any means for ensuring the precise microalignment of laser-ablated features in a miniaturized column device. Microalignment means can be formed in the column devices either by laser ablation or by other methods of fabricating shaped pieces well known in the art. Representative microalignment means that can be employed herein include a plurality of coaxially arranged apertures laser-ablated in component parts and/or a plurality of corresponding features in column device substrates, e.g., projections and mating depressions, grooves and mating ridges or the like. Further, the accurate microalignment of component parts can be effected by forming the miniaturized columns in flexible substrates having at least one fold means laser-ablated therein, such that sections of the substrate can be folded to overlie other sections thereby forming composite micro-scale compartments, aligning features such as apertures or detection means with separation compartments, or forming micro-scale separation compartments from microchannels. Such fold means can be embodied by a row of spaced-apart perforations ablated in a particular substrate, spaced-apart slot-like depressions or apertures ablated so as to extend only part way through the substrate, or the like. The perforations or depressions can have circular, diamond, hexagonal or other shapes that promote hinge formation along a predetermined straight line.

[0053] The term "liquid phase analysis" is used to refer to any analysis which is done on either small and/or macromolecular solutes in the liquid phase. Accordingly, "liquid phase analysis" as used herein includes chromatographic separations, electrophoretic separations, and electrochromatographic separations.

[0054] In this regard, "chromatographic" processes generally comprise preferential separations of components, and include reverse-phase, hydrophobic interaction, ion exchange, molecular sieve chromatography and like methods.

[0055] "Electrophoretic" separations refers to the migration of particles or macromolecules having a net electric charge where said migration is influenced by an electric field. Accordingly electrophoretic separations contemplated for use in the invention include separations performed in columns packed with gels (such as polyacrylamide, agarose and combinations thereof) as

well as separations performed in solution.

[0056] "Electrochromatographic" separation refers to combinations of electrophoretic and chromatographic techniques. Exemplary electrochromatographic separations include packed column separations using electromotive force (Knox et al. (1987) *Chromatographia* 24:135; Knox et al. (1989) *J. Liq. Chromatogr* 12:2435; Knox et al. (1991) *Chromatographia* 32:317), and micellar electrophoretic separations (Terabe et al. (1985) *Anal. Chem.* 57:834-841).

[0057] The term "motive force" is used to refer to any means for inducing movement of a sample along a column in a liquid phase analysis, and includes application of an electric potential across any portion of the column, application of a pressure differential across any portion of the column or any combination thereof.

[0058] The term "surface treatment" is used to refer to preparation or modification of the surface of a micro-channel which will be in contact with a sample during separation, whereby the separation characteristics of the device are altered or otherwise enhanced. Accordingly, "surface treatment" as used herein includes: physical surface adsorptions; covalent bonding of selected moieties to functional groups on the surface of micro-channel substrates (such as to amine, hydroxyl or carboxylic acid groups on condensation polymers); methods of coating surfaces, including dynamic deactivation of channel surfaces (such as by adding surfactants to media), polymer grafting to the surface of channel substrates (such as polystyrene or divinyl-benzene) and thin-film deposition of materials such as diamond or sapphire to microchannel substrates.

[0059] The term "laser ablation" is used to refer to a machining process using a high-energy photon laser such as an excimer laser to ablate features in a suitable substrate. The excimer laser can be, for example, of the F₂, ArF, KrCl, KrF, or XeCl type.

[0060] In general, any substrate which is UV absorbing provides a suitable substrate in which one may laser ablate features. Accordingly, under the present invention, microstructures of selected configurations can be formed by imaging a lithographic mask onto a suitable substrate, such as a polymer or ceramic material, and then laser ablating the substrate with laser light in areas that are unprotected by the lithographic mask.

[0061] In laser ablation, short pulses of intense ultraviolet light are absorbed in a thin surface layer of material within about 1 μ m or less of the surface. Preferred pulse energies are greater than about 100 millijoules per square centimeter and pulse durations are shorter than about 1 microsecond. Under these conditions, the intense ultraviolet light photo-dissociates the chemical bonds in the material. Furthermore, the absorbed ultraviolet energy is concentrated in such a small volume of material that it rapidly heats the dissociated fragments and ejects them away from the surface of the material. Because these processes occur so quickly, there is no time for heat to propagate to the surrounding material.

As a result, the surrounding region is not melted or otherwise damaged, and the perimeter of ablated features can replicate the shape of the incident optical beam with precision on the scale of about one micrometer.

[0062] Although laser ablation has been described herein using an excimer laser, it is to be understood that other ultraviolet light sources with substantially the same optical wavelength and energy density may be used to accomplish the ablation process. Preferably, the wavelength of such an ultraviolet light source will lie in the 150 nm to 400 nm range to allow high absorption in the substrate to be ablated. Furthermore, the energy density should be greater than about 100 millijoules per square centimeter with a pulse length shorter than about 1 microsecond to achieve rapid ejection of ablated material with essentially no heating of the surrounding remaining material. Laser ablation techniques, such as those described above, have been described in the art. Znotins, T.A., et al., *Laser Focus Electro Optics*, (1987) pp. 54-70; U.S. Patent Nos. 5,291,226 and 5,305,015 to Schantz et al.

[0063] The term "injection molding" is used to refer to a process for molding plastic or nonplastic ceramic shapes by injecting a measured quantity of a molten plastic or ceramic substrate into dies (or molds). In one embodiment of the present invention, miniaturized column devices may be produced using injection molding.

[0064] More particularly, it is contemplated to form a mold or die of a miniaturized column device wherein excimer laser-ablation is used to define an original microstructure pattern in a suitable polymer substrate. The microstructure thus formed may then be coated by a very thin metal layer and electroplated (such as by galvanofforming) with a metal such as nickel to provide a carrier. When the metal carrier is separated from the original polymer, an mold insert (or tooling) is provided having the negative structure of the polymer. Accordingly, multiple replicas of the ablated microstructure pattern may be made in suitable polymer or ceramic substrates using injection molding techniques well known in the art.

[0065] The term "LIGA process" is used to refer to a process for fabricating microstructures having high aspect ratios and increased structural precision using synchrotron radiation lithography, galvanofforming, and plastic molding. In a LIGA process, radiation sensitive plastics are lithographically irradiated at high energy radiation using a synchrotron source to create desired microstructures (such as channels, ports, apertures and micro-alignment means), thereby forming a primary template.

[0066] The primary template is then filled with a metal by electrodeposition techniques. The metal structure thus formed comprises a mold insert for the fabrication of secondary plastic templates which take the place of the primary template. In this manner highly accurate replicas of the original microstructures may be formed in a variety of substrates using injection or reactive injection molding techniques. The LIGA process has been

described by Becker, E.W., et al., *Microelectric Engineering* (1986) 4:35-56. Descriptions of numerous polymer substrates which may be injection molded using LIGA templates, and which are suitable substrates in the practice of the subject invention, may be found in "Contemporary Polymer Chemistry", Allcock, H.R. and Lampe, F.W. (Prentice-Hall, Inc.) New Jersey (1981).

[0067] "Optional" or "optionally" means that the subsequently described feature or structure may or may not be present in the μ -TAS or that the subsequently described event or circumstance may or may not occur, and that the description includes instances where said feature or structure is present and instances where the event or structure is absent, or instances where the event or circumstance occurs and instances where it does not. For example, the phrase "a μ -TAS optionally having detection means" intends that access ports may or may not be present on the device and that the description includes both circumstances where access ports are present and absent.

[0068] Accordingly, the invention concerns formation of miniaturized column devices including μ -TASs using laser ablation in a suitable substrate. It is also contemplated to form column devices and μ -TASs according to the invention using injection molding techniques wherein the original microstructure has been formed by an excimer laser ablation process, or where the original microstructure has been formed using a LIGA process.

[0069] More particularly, microstructures such as sample processing compartments, injection means, detection means and micro-alignment means may be formed in a planar substrate by excimer laser ablation. A frequency multiplied YAG laser may also be used in place of the excimer laser. In such a case, a complex microstructure pattern useful for practicing the invention may be formed on a suitable polymeric or ceramic substrate by combining a masking process with a laser ablation means, such as in a step-and-repeat process, where such processes would be readily understood by one of ordinary skill in the art.

[0070] In the practice of the invention, a preferred substrate comprises a polyimide material such as those available under the trademarks Kapton® or Upilex® from DuPont (Wilmington, Delaware), although the particular substrate selected may comprise any other suitable polymer or ceramic substrate. Polymer materials particularly contemplated herein include materials selected from the following classes: polyimide, polycarbonate, polyester, polyamide, polyether, polyolefin, or mixtures thereof. Further, the polymer material selected may be produced in long strips on a reel, and, optional sprocket holes along the sides of the material may be provided to accurately and securely transport the substrate through a step-and-repeat process.

[0071] According to the invention, the selected polymer material is transported to a laser processing chamber and laser-ablated in a pattern defined by one or more masks using laser radiation. In a preferred embod-

iment, such masks define all of the ablated features for an extended area of the material, for example encompassing multiple apertures (including inlet and outlet ports), micro-alignment means and sample processing chambers.

[0072] Alternatively, patterns such as the aperture pattern, the sample processing channel pattern, etc., may be placed side by side on a common mask substrate which is substantially larger than the laser beam. Such patterns may then be moved sequentially into the beam. In other contemplated production methods, one or more masks may be used to form apertures through the substrate, and another mask and laser energy level (and/or number of laser shots) may be used to define sample processing channels which are only formed through a portion of the thickness of the substrate. The masking material used in such masks will preferably be highly reflecting at the laser wavelength, consisting of, for example, a multilayer dielectric material or a metal such as aluminum.

[0073] The laser ablation system employed in the invention generally includes beam delivery optics, alignment optics, a high precision and high speed mask shuttle system, and a processing chamber including mechanism for handling and positioning the material. In a preferred embodiment, the laser system uses a projection mask configuration wherein a precision lens interposed between the mask and the substrate projects the excimer laser light onto the substrate in the image of the pattern defined on the mask.

[0074] It will be readily apparent to one of ordinary skill in the art that laser ablation may be used to form miniaturized sample processing channels and apertures in a wide variety of geometries. Any geometry which does not include undercutting may be provided using ablation techniques, such as modulation of laser light intensity across the substrate, stepping the beam across the surface or stepping the fluence and number of pulses applied to each location to control corresponding depth. Further, laser-ablated channels or chambers produced according to the invention are easily fabricated having ratios of channel depth to channel width which are much greater than previously possible using etching techniques such as silicon micromachining. Such aspect ratios can easily exceed unity, and may even reach to 10. Furthermore, the aspect ratio of laser-ablated channels and chambers can be less than one, i.e., the width of the channel or chamber can be greater than the depth.

[0075] In a preferred embodiment of the invention, channels of a semi-circular cross section are laser ablated by controlling exposure intensity or by making multiple exposures with the beam being reoriented between each exposure. Accordingly, when a corresponding semi-circular channel is aligned with a channel thus formed, a sample processing chamber of highly symmetrical circular cross-section is defined which may be desirable for enhanced fluid flow through the sample processing device.

[0076] As a final step in laser ablation processes contemplated by the invention, a cleaning step is performed wherein the laser-ablated portion of the substrate is positioned under a cleaning station. At the cleaning station, debris from the laser ablation are removed according to standard industry practice.

[0077] As will be appreciated by those working in the field of liquid phase analysis devices, the above-described method may be used to produce a wide variety of miniaturized devices. One such device is represented in Figure 1 where a miniaturized column device is generally indicated at **2**. Generally, miniaturized column **2** is formed in a selected substrate **4** using laser ablation techniques. The substrate **4** generally comprises first and second substantially planar opposing surfaces indicated at **6** and **8** respectively, and is selected from a material other than silicon which is UV absorbing and, accordingly, laser-ablatable.

[0078] The miniaturized column device **2** comprises a column structure ablated on a chip, which may be a machinable form of the plastic polyimide such as Vespel®. It is particularly contemplated to use such a polyimide substrate as, based on considerable experience with the shortcomings of fused silica and research into alternatives thereof, polyimides have proved to be a highly desirable substrate material for the analysis portion of a liquid phase sample processing system.

[0079] In this regard, it has been demonstrated that polyimides exhibit low sorptive properties towards proteins, which are known to be particularly difficult to analyze in prior silicon dioxide-based separation systems. Successful demonstrations of separations with this difficult class of solutes typically ensures that separation of other classes of solutes will be not be problematic. Further, since polyimide is a condensation polymer, it is possible to chemically bond groups to the surface which may provide a variety of desirable surface properties, depending on the target analysis. Unlike prior silicon dioxide based systems, these bonds to the polymeric substrate demonstrate pH stability in the basic region (pH 9-10).

[0080] Referring now to Figures 1-3, the substrate **4** has a microchannel **10** laser-ablated in a first planar surface **6**. It will be readily appreciated that, although the microchannel **10** has been represented in a generally extended form, microchannels may be ablated in a large variety of configurations, such as in a straight, serpentine, spiral, or any tortuous path desired. Further, as described in greater detail above, the microchannel **10** may be formed in a wide variety of channel geometries including semi-circular, rectangular, rhomboid, and the like, and the channels may be formed in a wide range of aspect ratios.

[0081] Referring particularly to Figures 1 and 4, a cover plate **12** is arranged over said first planar surface **6** and, in combination with the laser-ablated microchannel **10**, forms an elongate sample processing compartment **14**. Cover plate **12** may be formed from any suitable sub-

strate such as polyimide, the selection of the substrate only being limited by avoidance of undesirable separation surfaces such as silicon or silicon dioxide materials.

[0082] The cover plate **12** may be fixably aligned over the first planar surface **6** to form a liquid-tight sample processing compartment by using pressure sealing techniques, by using external means to urge the pieces together (such as clips, tension springs or associated clamping apparatus) or by using adhesives well known in the art of bonding polymers, ceramics and the like.

[0083] The cover plate **12** further comprises apertures ablated therein. In this regard, a first aperture communicates with the sample processing compartment **14** at a first end **16** thereof to form an inlet port **18** enabling the passage of fluid from an external source into said sample processing compartment. A second aperture communicates with the sample processing compartment **14** at a second end **20** thereof to form an outlet port **22** enabling passage of fluid from the sample processing compartment to an external receptacle. Accordingly, a miniaturized column device is formed having a flow path extending from the first end **16** of the sample processing compartment and passing to the second end **20** thereof, whereby liquid phase analysis of samples may be carried out using techniques well known in the art.

[0084] Referring still to Figures 1-4, a device is shown comprising sample introduction means laser-ablated into both the substrate **4** and cover plate **12**. An internally ablated by-pass channel **24** is formed in substrate **4**, said channel **24** being disposed near the first end **16** of the sample processing compartment. Two additional apertures **26** and **28** are formed in cover plate **12** and are arranged to cooperate with first and second ends (indicated at **30** and **32** respectively) of the by-pass channel **24**. In this manner, a sample being held in an external reservoir may be introduced into by-pass channel **24** to form a sample plug of a known volume (defined by the dimensions of the channel **24**). The sample plug thus formed may then be introduced into the first end **16** of the sample processing compartment **14** via inlet port **18** by communicating external mechanical valving with said inlet port and laser-ablated apertures **26** and **28** and flushing solution through the by-pass channel **24** into the sample processing compartment.

[0085] It is noted that the ablated by-pass channel **24** and apertures **26** and **28** further enable a wide variety of sample introduction techniques to be practiced according to the invention. Particularly, having a by-pass channel which is not connected to the sample processing compartment allows a user to flush a sample through the by-pass channel without experiencing sample carry-over or column contamination. As will be appreciated by one of ordinary skill in the art after reading this specification, one such sample introduction technique may be effected by butt-coupling an associated rotor to a stator (not shown) on the external surface of a miniaturized column where the rotor selectively interfaces external

tubing and fluid sources with inlet port **18** and apertures **26** and **28**, allowing a sample to be flushed from the by-pass channel **24** into external tubing from which the sample may then be introduced into the column via inlet port **18** for liquid phase analysis thereof. In this regard, a miniaturized column device formed in a polyimide substrate enables a ceramic rotor, pressed to the device using tensioned force (to form a liquid-tight seal), to still rotate between selected aperture positions on the device due to the friction characteristics of the two materials. Other suitable rotors can be formed in rigid materials such as, but not limited to, glass and non-conductive substrates.

[0086] Accordingly, external hardware provides the mechanical valving necessary for communication of a miniaturized column device to different external liquid reservoirs, such as an electrolyte solution, flush solution or the sample via laser-ablated holes designed into the cover plate **12**. This feature allows a variety of injection methods to be adapted to a miniaturized planar column device including pressure injection, hydrodynamic injection or electrokinetic injection. In the device of Figures 1-3, it is contemplated that external valving and injection means communicate with the sample processing device by butt-coupling to the laser-ablated apertures, however, any other suitable methods of connection known in the art may easily be adapted to the invention.

[0087] A wide variety of means for applying a motive force along the length of the sample processing compartment **14** may be associated with the subject device. In this regard, a pressure differential or electric potential may be applied along the entire length of the sample processing compartment by interfacing motive means with inlet port **18** and outlet port **22**.

[0088] The use of substrates such as polyimides in the construction of miniaturized columns allows the possibility of using refractive-index (RI) detection to detect separated analytes of interest passing through the subject columns. In this regard, the provision of an associated laser diode which emits radiation at a wavelength where polyimide is "transparent" (such as at >500 nm) allows for a detection setup where no additional features need to be ablated in the column devices.

[0089] Referring now to Figures 2-4, detection means may be ablated into the substrate **4** and cover plate **12**, where said detection means is disposed substantially downstream of the first end **16** of the sample processing compartment **14**. More particularly, an aperture **34** may be ablated through substrate **4** to communicate with the sample processing compartment **14**. A corresponding aperture **36** may be likewise formed in cover plate **12**, and arranged so that it will be in co-axial alignment with aperture **34** when the cover plate is affixed to the substrate to form the sample processing compartment **14**. In this manner, electrodes (not shown) may be connected to the miniaturized column device via the apertures **34** and **36** to detect separated analytes of interest passing through the sample processing compart-

ment by electrochemical detection techniques.

[0090] Referring to Figure 5, a further device indicated at **2'** is shown comprising a preferred detection means indicated generally at **42**. More particularly, a first transparent sheet **38** is provided wherein the cover plate **12** is interposed between said first transparent sheet and substrate **4**. A second transparent sheet **40** is also provided wherein the second sheet is disposed over the second planar surface **8** of the substrate **4**. In this manner, detection means **42** allows optical detection of separated analytes passing through sample processing compartment, formed by the combination of microchannel **10** and cover plate **12**, via transmission of radiation orthogonal to the major axis of the sample processing compartment (and, accordingly, orthogonal to the direction of electro-osmotic flow in an electrophoretic separation). Further, the transparent sheets may comprise materials such as quartz, diamond, sapphire, fused silica or any other suitable substrate which enables light transmission therethrough.

[0091] The subject transparent sheets may be formed with just enough surface area to cover and seal the detection apertures **34** and **36**, or said sheets may be sized to cover up to the entire surface area of the column device. In this regard, additional structural rigidity may be provided to a column device formed in a particularly thin substrate film, such as a thin-film polyimide substrate, by employing a substantially coplanar sheet of, for example, fused silica.

[0092] Accordingly, the above described optical detection means **42** enables adaptation of a variety of external optical detection means to miniaturized columns. Further, sealing of the transparent sheets **38** and **40** to the miniaturized column device **2'** is readily enabled, for example, when substrate **4** and cover plate **12** are formed in polyimide materials which include a layer of a thermal adhesive form of polyimide, since it is known that quartz/Kapton® bonds formed using such adhesives are very resilient. Sealing of other preferred transparent sheet materials, such as diamond, sapphire or fused-silica to the subject device may be accomplished using adhesion techniques well known in the art.

[0093] The possibility of detecting with radiation over a range of electromagnetic wavelengths offers a variety of spectrophotometric detection techniques to be interfaced with a miniaturized column according to the invention, including UV/Vis, fluorescence, refractive index (RI) and Raman.

[0094] Furthermore, as will be readily appreciated, the use of optical detection means comprising apertures ablated into the substrate and cover plate provides great control over the effective detection path length in a miniaturized column device. In this regard, the detection path length will be substantially equal to the combined thickness of the substrate **4** and the cover plate **12**, and detection path lengths of up to 250 μm readily obtainable using the subject detection means **42** in thin-film substrates such as polyimides.

[0095] Referring now to Figure 6, it can be seen that apertures **34** and **36** provide an enlarged volume in sample processing compartment **14** at the point of intersection with the detection means **42**, where that volume will be proportional to the combined thickness of substrate **4** and cover plate **12**. In this manner, sample plugs passing through sample processing compartment **14** may be subject to untoward distortion as the plug is influenced by the increased compartment volume in the detection area, especially where the combined thickness of the substrate and cover plate exceeds about 250 μm , thereby possibly reducing separation efficiency in the device.

[0096] Accordingly, if detection path lengths exceeding 250 μm are desired, an alternative device is provided having laser-ablated features on two opposing surfaces of a substrate. More particularly, in Figures 7A and 7B, a miniaturized column device is generally indicated at **52**. The miniaturized column comprises a substrate **54** having first and second substantially planar opposing surfaces respectively indicated at **56** and **58**. The substrate **54** has a first microchannel **60** laser ablated in the first planar surface **56** and a second microchannel **62** laser ablated in the second planar surface **58**, wherein the microchannels can be provided in a wide variety of geometries, configurations and aspect ratios as described above.

[0097] The miniaturized column device of Figures 7A and 7B further includes first and second cover plates, indicated at **64** and **66** respectively, which, in combination with the first and second microchannels **60** and **62**, define first and second elongate separation compartments when substrate **54** is sandwiched between the first and second cover plates.

[0098] Referring still to Figures 7A and 7B, a plurality of apertures can be laser-ablated in the device to provide an extended separation compartment, and further to establish fluid communication means. More particularly, a conduit means **72**, comprising a laser ablated aperture in substrate **54** having an axis which is orthogonal to the first and second planar surfaces **56** and **58**, communicates a distal end **74** of the first microchannel **60** with a first end **76** of the second microchannel **62** to form an extended separation compartment.

[0099] Further, an aperture **68**, laser ablated in the first cover plate **64**, enables fluid communication with the first microchannel **60**, and a second aperture **70**, laser ablated in the second cover plate **66**, enables fluid communication with the second microchannel **62**. As will be readily appreciated, when the aperture **68** is used as an inlet port, and the second aperture **70** is used as an outlet port, a miniaturized column device is provided having a flow path extending along the combined length of the first and second microchannels **60** and **62**.

[0100] In the device as shown in Figures 7A and 7B, a wide variety of sample introduction means can be employed, such as those described above. External hardware can also be interfaced to the subject device to provide liquid handling capabilities, and a variety of means

for applying a motive force along the length of the separation compartment can be associated with the device, such as by interfacing motive means with the first and/or second apertures **68** and **70** as described above.

[0101] Additionally, a variety of detection means are easily included in the subject device. In this regard, a first aperture **78** can be laser ablated in the first cover plate **64**, and a second aperture **80** can likewise be formed in the second cover plate **66** such that the first and second apertures will be in co-axial alignment with conduit means **72** when the substrate **54** is sandwiched between the first and second cover plates. Detection of analytes in a separated sample passing through the conduit means is thereby easily enabled, such as by connecting electrodes to the miniaturized column via apertures **78** and **80** and detecting using electrochemical techniques.

[0102] However, a key feature of the laser-ablated conduit means **72** is the ability to provide an extended optical detection path length of up to 1 mm, or greater, without experiencing untoward sample plug distortion due to increased separation compartment volumes at the point of detection. Referring to Figures 7A, 7B and 9, first and second transparent sheets, indicated at **82** and **84** respectively, can be provided such that the first cover plate **64** is interposed between the first transparent sheet and the first planar surface **56**, and the second cover plate **66** is interposed between the second transparent sheet and the second planar surface **58**. The transparent sheets **82** and **84** can be selected from appropriate materials such as quartz crystal, fused silica, diamond, sapphire and the like. Further, the transparent sheets can be provided having just enough surface area to cover and seal the apertures **78** and **80**, or those sheets can be sized to cover up to the entire surface area of the column device. As described above, this feature allows additional structural rigidity to be provided to a column device formed in a particularly thin substrate.

[0103] As best shown in Figure 9, the subject arrangement allows optical detection of sample analytes passing through the miniaturized column device to be carried out along an optical detection path length **86** corresponding to the major axis of the conduit means **72**. As will be readily appreciated, the optical detection path length **86** is substantially determined by the thickness of the substrate **54**, and, accordingly, a great deal of flexibility in tailoring a miniaturized column device having μ -meter column dimensions and optical path lengths of up to 1 mm or greater is thereby enabled under the instant invention. In this manner, a wide variety of associated optical detection devices may be interfaced with a miniaturized column, and detection of analytes in samples passing through the conduit means **72** may be carried out using UV/Vis, fluorescence, refractive index (RI), Raman and like spectrophotometric techniques.

[0104] Referring now to Figures **8A** and **8B**, a related device is shown, comprising a miniaturized column device **52'**, wherein the column portion and the first and

second cover plates are formed in a single, flexible substrate generally indicated at **88**. The flexible substrate **88** thus comprises three distinct regions, a column portion **88B**, having first and second substantially planar opposing surfaces **56'** and **58'**, respectively, where the column portion is interposed between a first cover plate portion **88A** and a second cover plate portion **88C**. The first and second cover plate portions have at least one substantially planar surface. The first cover plate portion **88A** and the column portion **88B** are separated by at least one fold means **90** such that the first cover plate portion can be readily folded to overlie the first substantially planar surface **56'** of the column portion **88B**. The second cover plate portion **88C** and the column portion **88B** are likewise separated by at least one fold means **92** such that the second cover plate can her readily folded to overlie the second substantially planar surface **58'** of the column portion **88B**. Each fold means **90** and **92** can comprise a row of spaced-apart perforations ablated in the flexible substrate, spaced-apart slot-like depressions or apertures ablated so as to extend only part way through the substrate, or the like. The perforations or depressions can have circular, diamond, hexagonal or other shapes that promote hinge formation along a predetermined straight line.

[0105] Thus, the miniaturized column device **52'** is formed by laser ablating a first microchannel **60'** in the first planar surface **56'** of the column portion **88B**, and a second microchannel **62'** in the second planar surface **58'** of the column portion. Each microchannel can be provided in a wide variety of geometries, configurations and aspect ratios. A first separation compartment is then formed by folding the flexible substrate **88** at the first fold means **90** such that the first cover plate portion **88A** covers the first microchannel **60'** to form an elongate separation compartment. A second separation compartment is then provided by folding the flexible substrate **88** at the second fold means **92** such that the second cover plate portion **88C** covers the second microchannel **62'** to form a separation compartment as described above. A conduit means **72'**, comprising a laser ablated aperture in the column portion **88B** having an axis which is orthogonal to the first and second planar surfaces **56'** and **58'**, communicates a distal end of the first microchannel **60'** with a first end of the second microchannel **62'** to form a single, extended separation compartment.

[0106] Further, an aperture **68'**, laser ablated in the first cover plate portion **88A**, enables fluid communication with the first microchannel **60'**, and a second aperture **70'**, laser ablated in the second cover plate portion **88C**, enables fluid communication with the second microchannel **62'**. As described above, when the first and second apertures are used as an inlet and outlet port, respectively, a miniaturized column device is provided having a flow path extending along the combined length of the first and second microchannels.

[0107] Detection means can optionally be included in the device of Figures **8A** and **8B**. A first aperture **78'** can

be laser ablated in the first cover plate portion **88A**, and a second aperture **80'** can likewise be formed in the second cover plate portion **88C**, wherein the apertures are arranged to co-axially communicate with each other and communicate with the conduit means **72'** when the flexible substrate **88** is hingeably folded as described above to accurately align the apertures **78'** and **80'** with the conduit means **72'**.

[0108] Optional micro-alignment means--formed either by laser ablation techniques or by other methods of fabricating shaped pieces well known in the art--are provided in the miniaturized column device **52'**. More specifically, a plurality of corresponding laser-ablated apertures (not shown) can be provided in the column portion **88B** and the first and second cover plate portions, **88A** and **88C**, respectively of the flexible substrate **88**. The subject apertures are arranged such that co-axial alignment thereof enables the precise alignment of the column portion with one, or both of the cover plate portions to align various features such as the optional detection means with the ablated conduit. Such optional alignment can be effected using an external apparatus with means (such as pins) for cooperating with the co-axial apertures to maintain the components are portions in proper alignment with each other.

[0109] Accordingly, novel miniaturized column devices have been described which are laser ablated into a substrate other than silicon or silicon dioxide materials, and which avoid several major problems which have come to be associated with prior attempts at providing micro-column devices. The use of laser ablation techniques enables highly symmetrical and accurately defined micro-column devices to be fabricated in a wide class of polymeric and ceramic substrates to provide a variety of miniaturized liquid-phase analysis systems. In this regard, miniaturized columns may be provided which have micro-capillary dimensions (ranging from 5-200 μm in diameter) and column detection path lengths of up to 1 mm or greater. This feature has not been attainable in prior attempts at miniaturization, such as in capillary electrophoresis, without substantial engineering of a device after capillary formation. Further, laser ablation of miniaturized columns in inert substrates such as polyimides avoids the problems encountered in prior devices formed in silicon or silicon dioxide-based materials. Such problems include the inherent chemical activity and pH instability of silicon and silicon dioxide-based substrates which limits the types of separations capable of being performed in those devices.

[0110] Miniaturized column devices may be formed by laser ablating a set of desired features in a selected substrate using a step-and-repeat process to form discrete units. In this regard, it is particularly contemplated to laser ablate the subject devices in condensation polymer substrates including polyimides, polyamides, polyesters and polycarbonates. Further, it is contemplated to use either a laser ablation process or a LIGA process to form templates encompassing a set of desired fea-

tures, whereby multiple copies of miniaturized columns may be mass-produced using injection molding techniques well known in the art. More particularly, it is contemplated herein to form miniaturized columns by injection molding in substrates comprised of materials such as the following: polycarbonates; polyesters, including poly(ethylene terephthalate) and poly(butylene terephthalate); polyamides, (such as nylons); polyethers, including polyformaldehyde and poly(phenylene sulfide); polyimides, such as Kapton® and Upilex®; polyolefin compounds, including ABS polymers, Kel-F copolymers, poly(methyl methacrylate), poly(styrene-butadiene) copolymers, poly(tetrafluoroethylene), poly(ethylene-vinyl acetate) copolymers, poly(N-vinylcarbazole) and polystyrene.

[0111] Laser ablation of microchannels in the surfaces of the above-described substrates has the added feature of enabling a wide variety of surface treatments to be applied to the microchannels before formation of the sample processing compartment. That is, the open configuration of laser-ablated microchannels enables a number of surface treatments or modifications to be performed which are not possible in closed format constructions, such as in prior micro-capillaries. More specifically, laser ablation in condensation polymer substrates provides microchannels with surfaces featuring functional groups, such as carboxyl groups, hydroxyl groups and amine groups, thereby enabling chemical bonding of selected species to the surface of the subject microchannels using techniques well known in the art. Other surface treatments enabled by the open configuration of the instant devices include surface adsorptions, polymer graftings and thin film deposition of materials such as diamond or sapphire to microchannel surfaces using masking and deposition techniques and dynamic deactivation techniques well known in the art of liquid separations.

[0112] The ability to exert rigid computerized control over the present laser ablation processes enables extremely precise microstructure formation, which, in turn, enables the formation of miniaturized columns having features ablated in two substantially planar components wherein those components may be aligned to define a composite sample processing compartment of enhanced symmetry and axial alignment. In this regard, it is contemplated to use laser ablation to create two component halves which, when folded or aligned with one another, define a single miniaturized column device.

[0113] Referring now to Figure 10, a miniaturized column for liquid phase analysis of a sample is generally indicated at **102**. The miniaturized column **102** is formed by providing a support body **104** having first and second component halves indicated at **106** and **108** respectively. The support body may comprise a substantially planar substrate such as a polyimide film which is both laser ablatable and flexible so as to enable folding after ablation; however, the particular substrate selected is not considered to be limiting in the invention.

[0114] The first and second component halves **106** and **108** each have substantially planar interior surfaces, indicated at **110** and **112** respectively, wherein miniaturized column features may be laser ablated. More particularly, a first microchannel pattern **114** is laser ablated in the first planar interior surface **110** and a second microchannel pattern **116** is laser ablated in the second planar interior surface **112**. According to the invention, said first and second microchannel patterns are ablated in the support body **104** so as to provide the mirror image of each other.

[0115] Referring now to Figures 11 and 12, a sample processing compartment **118**, comprising an elongate bore defined by the first and second microchannel patterns **114** and **116** may be formed by aligning (such as by folding) the first and second component halves **106** and **108** in facing abutment with each other. In the practice of the invention, the first and second component halves may be held in fixable alignment with one another to form a liquid-tight sample processing compartment using pressure sealing techniques, such as by application of tensioned force, or by use of adhesives well known in the art of liquid phase separation devices. It is further contemplated according to the invention to form first and second microchannels **114** and **116** having semi-circular cross-sections whereby alignment of the component halves defines a sample processing compartment **118** having a highly symmetrical circular cross-section to enable enhanced fluid flow therethrough; however, as discussed above, a wide variety of microchannel geometries are also within the spirit of the invention.

[0116] In a further preferred embodiment of the invention, it is particularly contemplated to form the support body **104** from a polymer laminate substrate comprising a Kapton® film co-extruded with a thin layer of a thermal plastic form of polyimide referred to as KJ® and available from DuPont (Wilmington, Delaware). In this manner, the first and second component halves **106** and **108** may be heat sealed together, resulting in a liquid-tight weld that has the same chemical properties and, accordingly, the same mechanical, electrical and chemical stability, as the bulk Kapton® material.

[0117] Referring now to Figures 10-12, the miniaturized column device **102** further comprises means for communicating associated external fluid containment means (not shown) with the sample processing compartment **118** to provide a liquid-phase separation device. More particularly, a plurality of apertures may be laser ablated in the support body **104**, wherein said apertures extend from at least one exterior surface of the support body and communicate with at least one microchannel, said apertures permitting the passage of fluid therethrough. In this regard, an inlet port **120** may be laser ablated in the first component half **106** and communicate with a first end **122** of said first microchannel **114**. In the same manner, an outlet port **124** may be ablated in the first component half and communicate with

a second end **126** of said first microchannel **114**.

[0118] As is readily apparent, a liquid phase sample processing device may thereby be formed, having a flow path extending from the first end **122** of the microchannel **114** to the second end **126** thereof, by communicating fluids from an associated source (not shown) through the inlet port **120**, passing the fluids through the sample processing compartment **118** formed by the alignment of microchannels **114** and **116**, and allowing the fluids to exit the sample processing compartment via the outlet port **126**. In this manner, a wide variety of liquid phase analysis procedures may be carried out in the subject miniaturized column device using techniques well known in the art. Furthermore, various means for applying a motive force along the length of the sample processing compartment **118**, such as a pressure differential or electric potential, may be readily interfaced to the column device via the inlet and outlet ports, or by interfacing with the sample processing compartment via additional apertures which may be ablated in the support body **104**.

[0119] Inlet port **120** may be formed such that a variety of external fluid and/or sample introduction means may be readily interfaced with the miniaturized column device **102**. As discussed in greater detail above, such means include external pressure injection, hydrodynamic injection or electrokinetic injection mechanisms.

[0120] Referring now to Figures 10 and 11, the miniaturized column device **102** further comprises detection means laser ablated in the support body **104**. More particularly, a first aperture **128** is ablated in said first component half **106** and communicates with the first microchannel **114** at a point near the second end **126** thereof. A second aperture **130** is likewise formed in said second component half **108** to communicate with the second microchannel **116**. Accordingly, a wide variety of associated detection means may then be interfaced to the sample processing compartment **118** to detect separated analytes of interest passing therethrough, such as by connection of electrodes to the miniaturized column via the first and second apertures **128** and **130**.

[0121] In yet a further preferred embodiment of the invention, an optical detection means is provided in the miniaturized column device **102**. In this regard, first and second apertures **128** and **130** may be ablated in the support body **104** such that when the component halves are aligned to form the sample processing compartment **118** said apertures are in co-axial alignment with one another, said apertures further having axes orthogonal to the plane of said support body. As will be readily appreciated by one of ordinary skill in the art, by providing transparent sheets (not shown), disposed over the exterior of the support body **104** and covering said first and second apertures **128** and **130**, a sample passing through sample processing compartment **118** may be analyzed by interfacing spectrophotometric detection means with said sample through the transparent sheets using techniques well known in the art. The optical de-

tection path length may be substantially determined by the combined thickness of said first and second component halves **106** and **108**. In this manner, an optical detection path length of up to **250** μm is readily provided by ablating the miniaturized column device in a **125** μm polymer film.

[0122] Accordingly, there have been described several preferred embodiments of a miniaturized column device formed according to the invention by laser ablating microstructures on component parts and aligning the components to form columns having enhanced symmetries. As described in detail above, formation of the subject microchannels in the open configuration enables a wide variety of surface treatments and modifications to be applied to the interior surfaces of the channels before formation of the sample processing compartment. In this manner, a wide variety of liquid phase analysis techniques may be carried out in the composite sample processing compartments thus formed, including chromatographic, electrophoretic and electrochromatographic separations.

[0123] In the practice of the invention, it is further contemplated to provide optional means for the precise alignment of component support body halves, thereby ensuring accurate definition of a composite sample processing compartment formed according to the invention. More particularly, in a further preferred embodiment of the invention, micro-alignment means are provided to enable enhanced alignment of laser-ablated component parts such as microchannels, detection apertures and the like.

[0124] Referring now to Figures 13 and 14, a miniaturized column device constructed according to the present invention is generally indicated at **150** and is formed in a flexible substrate **152**. The column device comprises first and second support body halves, indicated at **154** and **156** respectively, each having a substantially planar interior surface indicated at **158** and **160** respectively. The interior surfaces comprise laser-ablated microstructures, generally indicated at **162**, where said microstructures are arranged to provide the mirror image of one another in the same manner as described in greater detail above.

[0125] The accurate alignment of component parts may be enabled by forming a miniaturized column device in a flexible substrate **152** having at least one fold means, generally indicated at **180**, such that a first body half **154** may be folded to overlie a second body half **156**. The fold means **180** may comprise a row of spaced-apart perforations ablated in the substrate **152**, spaced-apart slot-like depressions or apertures ablated so as to extend only part way through the substrate, or the like. The perforations or depressions may have circular, diamond, hexagonal or other shapes that promote hinge formation along a predetermined straight line.

[0126] Accordingly, in the practice of the invention, the fold means **180** allows said first and second support body halves **154** and **156** to hingeably fold upon one

another and accurately align composite features defined by said microstructures ablated on said first and second planar interior surfaces **158** and **160**.

[0127] It is further contemplated to provide additional micro-alignment means formed either by laser ablation or by other methods of fabricating shaped pieces well known in the art. More specifically, a plurality of laser-ablated apertures (not shown) may be provided in said first and second support body halves **154** and **156** where said apertures are so arranged such that co-axial alignment thereof enables the precise alignment of the support body halves to define composite features such as an ablated elongate bore. Alignment may be effected using an external apparatus with means (such as pins) for cooperating with said co-axial apertures to maintain the body halves in proper alignment with one another.

[0128] Referring to Figures 13 and 14, in yet another particular embodiment of the invention, micro-alignment means may be formed in said first and second support body halves **154** and **156** using fabrication techniques well known in the art e.g., molding or the like. In this manner, a plurality of projections, indicated at **164**, **166** and **168**, may be formed in said first support body half **154**. A plurality of depressions, indicated at **170**, **172** and **174**, may be formed in said second support body half **156**.

[0129] Accordingly, as is readily apparent, the micro-alignment means are configured to form corresponding structures with one another, whereby projection **164** mates with depression **170**, projection **166** mates with depression **172**, and projection **168** mates with depression **174** when said support body halves are aligned in facing abutment with one another. In this manner, positive and precise alignment of support body halves **154** and **156** is enabled, thereby accurately defining composite features defined by said laser-ablated microstructures **162**.

[0130] As will be readily apparent to one of ordinary skill in the art after reading this specification, a wide variety of corresponding micro-alignment features may be formed in the subject miniaturized column devices without departing from the spirit of the instant invention. Such additional features include any combination of holes and/or corresponding structures such as grooves and ridges in said component parts where said features cooperate to enable precise alignment of the component body parts.

[0131] Figure 15 illustrates one embodiment of a μ -TAS. While this embodiment is described for bioanalytical applications (see Example 1), it is desired to provide start-to-finish analysis for any solute species, including small (less than about 1000 molecular weight) and large (greater than about 1000 molecular weight) solute species in complex matrices.

[0132] Generally, μ -TAS **200** may be constructed by providing a support body having first and second component halves with planar interior surfaces, laser ablating mirror images of a microchannel having more than

one sample handling region (202 through 212 and 214 through 220) in the interior surfaces of the first and second component interior surfaces, and optionally having laser-ablated access ports (222 through 232) and detection means (234 through 240). A sample processing compartment having sample flow components (202 through 212) and sample treatment components (214 through 220) may be formed by aligning the interior surfaces in facing abutment with each other (*see, e.g.*, Figures 10-12).

[0133] Mirror images of a microchannel having more than one sample handling region (202 through 212 and 214 through 220) can be laser ablated in the first planar surface of the column portion and the interior surface of the first cover portion of the flexible substrate such that a sample processing compartment is formed by folding the flexible substrate at the first fold means as described above by aligning the first planar surface of the column portion with the interior surface of the first cover portion in facing abutment with each other.

[0134] Generally, the sample handling region of the microchannel from which the sample flow components (202 through 212) are formed is elongate and semi-circular in geometry. However, as described in greater detail above, the microchannel may be formed in a wide variety of channel geometries including semi-circular, rectangular, rhomboid, and the like, and the channels may be formed in a wide range of aspect ratios. The sample handling region of the microchannel from which the sample treatment components (214 through 220) are formed is typically rectangular; however, it may be laser ablated in any desired geometry. Furthermore, in any particular μ -TAS, the sample handling regions of the microchannel may be formed in any combination of geometries including rectangular, square, triangular, and the like. In addition, while the μ -TAS illustrated in Figure 15 contains sample flow components with high aspect ratios (*i.e.*, aspect ratios in which the depth of the microstructure is greater than the width) and sample treatment components with low aspect ratios (*i.e.*, aspect ratios in which the width of the microstructure is greater than the depth), this is not intended to be limiting. For example, sample treatment components may have high aspect ratios, as in fourth sample treatment component 220.

[0135] As depicted in Figure 15, μ -TAS 200 is a serial arrangement of alternating sample flow components 202 through 212 and sample treatment components 214 through 220. Optionally, detection means 232 through 240 are disposed along the sample flow components. The detection means may be formed in the cover plate, the substrate itself, or both the cover plate and the substrate, as described in greater detail above.

[0136] In addition, optional access ports (222 through 232) depicted in Figure 15 are disposed along the sample flow components. The access ports allow the fluid communication of the sample flow component with, for example, external liquid reservoirs or mechanical val-

ing necessary for the introduction or removal of samples, buffers and the like from the sample flow component as required to effect sample preparation by the μ -TAS. External hardware may also be interfaced to the subject μ -TAS to provide liquid handling capabilities, and a variety of means for applying a motive force along the length of the sample processing compartment may be associated with the μ -TAS. Thus, access ports may be in divertable and switchable fluid communication with a valving manifold such that a valve in communication with an access port can be individually "actuated," *i.e.*, opened to allow flow or closed to prevent flow through the access port.

[0137] In particular reference to Figure 15, μ -TAS 200 depicted therein contains first access port 222 by which sample may be introduced into first sample flow component 202 that is in fluid communication with first sample treatment component 214. The sample may be directly added to the sample flow component via first access port 222 without prior processing. Optionally, first access port 222 may be interfaced with an external pre-column sample preparation device, *e.g.*, a filtration device.

[0138] In one embodiment, sample treatment component 214 performs a filtration function and may be filled with a porous medium made of particles, sheets or membranes. In a preferred embodiment, the medium has an effective pore size of between 45 μ m and 60 μ m. Preferably, the medium is biocompatible and may be made from such materials as nylon, cellulose, polymethylmethacrylate, polyacrylamide, agarose, or the like. In an alternative embodiment, the filtration function may be performed by an in-line device prior to introduction of the sample into sample flow component 214.

[0139] In the particular embodiment depicted in Figure 15, sample treatment component 214 is designed to serve a "capture" function. Thus, sample treatment component 214 can be an affinity chromatography, ion exchange chromatography, a complexation reaction or any such quantal chromatographic technique (*i.e.*, a chromatographic technique that could otherwise be performed in a batch mode rather than with a flowing sample stream). An affinity chromatography matrix may include a biological affiant, an antibody, a lectin, enzyme substrate or analog, enzyme inhibitor or analog, enzyme cofactor or analog, a capture oligonucleotide, or the like, depending on the nature of the sample. The ion exchange matrix may be an anionic or cationic ion exchange medium. Complexation reactions may include boronate reactions, dithiol reactions, metal-ion reactions, for example, with porphyrin or phenanthroline, or other reactions in which the sample is reversibly reacted with the chromatography matrix.

[0140] First and second access ports 222 and 224 are respectively disposed upstream and downstream from first sample treatment component 214. When first access port 222 is used as an input port and second access port 224 is used as a withdrawal port, sample treatment component 214 can be isolated from downstream

μ -TAS sample handling regions. Thus, while a sample is loaded onto sample treatment component **214**, extraneous materials which are flushed from the sample treatment component during analyte capture may be withdrawn and, in this manner, prevented from entering downstream μ -TAS sample handling regions. Alternatively, second access port **224** may be used as an fluid input port to provide flow regulation, sample derivatization, or other like function when connected to a source of fluid which may be an external fluid source or an on-device fluid reservoir compartment (see Figure 16).

[0141] Once a sample has been introduced into first sample flow component **214**, sample flow may be effected by way of an external motive means which is interfaced with first access port **222**. Alternatively, sample flow into sample treatment component **214** may be effected by activation of an on-device motive means, e.g., an on-device fluid reservoir compartment.

[0142] First detection means **234** may be in direct or indirect communication with second sample flow component **204** downstream from first sample treatment component **214**. First detection means **234** can be used to monitor the presence of a sample in sample flow component **204** which is to be loaded onto second sample treatment component **216** or to monitor sample elution from first sample treatment component **214**. In the latter case, it is preferred that first detection means **234** is placed in second sample flow component **204** upstream from second access port **224**.

[0143] In the particular embodiment depicted in Figure 15, second sample treatment component **216** serves to desalt or neutralize the analyte eluted from first sample treatment component **214**. Thus, second sample treatment component **216** may be an electrophoretic desalting, pH neutralizing, size exclusion chromatography component, or the like.

[0144] As with first sample treatment component **214**, second sample treatment component **216** is flanked by second and third access ports **224** and **226**. First, second and third access ports **222**, **224** and **226** may be used in any combination of inlet and outlet ports. Generally, once the sample has been eluted from first sample treatment component **214** and loaded onto second sample treatment component **216**, second access port **224** serves as an inlet port and third access port **226** serves as an outlet port, thereby isolating second sample treatment component **216** from downstream μ -TAS sample handling regions. In order to prevent backflow into first sample treatment component **214**, first access port **222** can be closed.

[0145] As exemplified in Figure 15, third sample treatment component **218** has been configured as an analyte focussing and pre-final sample processing compartment. As such, third sample treatment component **218** can be an isoelectric focusing component, an isotachopheric sample stacking component, or the like. Again, third sample treatment component **218** is flanked by third and fourth access ports **226** and **228**, which may

be operated in a manner similar to that described for access port pairs **222/224** and **224/226** to isolate third sample treatment component **218** from downstream sample handling regions. Second and third detection means **236** and **238** may also be used as described above for first detection means **234**.

[0146] Fourth sample treatment component **220** may include single or multiple functions selected from chromatographic, electrophoretic, or electrochromatographic functions. Although only one sample treatment component **220** is shown in Figure 15, multiple components of various dimensions can be laser ablated in continuum and specifically prepared as different sample processing functions in series. Examples of chromatographic functions which may be included in fourth sample treatment component **220** are reverse phase chromatography, hydrophobic interaction chromatography, affinity chromatography, size exclusion chromatography, ion exchange chromatography, chiral separation chromatography, and the like. For chromatographic functions, the stationary phase may be bonded or otherwise adhered to the surface of a particle or to the walls of the component. Examples of electrophoretic chromatography include open tubular electrophoresis, micellar electrokinetic capillary electrophoresis (see, Terabe et al. (1985) *Anal. Chem.* **57**:834-841), capillary chiral electrophoresis, and the like. Open tubular electrophoresis includes bonded phase, dynamic deactivation using any of a variety of inorganic or organic reagents, isoelectric focussing, and the like. Micellar electrokinetic capillary chromatography may be done using surfactants such as sodium dodecyl sulfate, cetyl ammonium bromide, alkyl glucosides, alkyl maltosides, zwitterionic surfactants such as 3-[(3-cholamidopropyl)-dimethylammonio]-1-propane sulfonate ("CHAPS"), 3-[(3-cholamidopropyl)-dimethylammonio]-2-hydroxy-1-propane sulfonate ("CHAPSO"), or the like. Capillary chiral electrophoresis may be done using reagents such as cyclodextrins, crown ethers, bile salts, or the like.

[0147] Fourth detection means **240** can be situated in the sample flow component that is downstream from fourth sample treatment component **220**. The detection means may be ablated into the substrate, cover plate, or both the substrate and the cover plate.

[0148] optionally, as illustrated and described in detail in reference to Figures 7 and 8, fourth detection means **240** may be conduit means **72** comprising a laser-ablated aperture in the substrate **54** having an axis which is orthogonal to the first **56** and second **58** planar surfaces of the substrate, and communicating a distal end **74** of the sample processing compartment **60** with a first end **76** of a second microchannel **62** to form an extended sample processing compartment. As depicted in Figure 9, this arrangement allows optical detection of sample analytes passing through the μ -TAS to be carried out along an optical detection path length **86** corresponding to the major axis of the conduit means **72**. In this manner, a wide variety of associated optical detection devices

es may be interfaced with a μ -TAS constructed according to the invention, thereby allowing detection of analytes in samples passing through the conduit means **72** using UV/Vis, fluorescence, refractive index (RI), Raman and like spectrophotometric techniques.

[0149] In a further optional embodiment of the μ -TAS, fifth access port **230** may serve one or more of a number of functions. As described above, fifth access port **230** may serve as an outlet port for fourth sample treatment component **220**. It may optionally be attached to an external or on-device fluid reservoir compartment, thereby providing a means to regulate sample flow rates through the μ -TAS or a means to introduce reagents into fifth sample flow component **210** which react with the sample to facilitate sample detection by fourth detection means **240**'.

[0150] Sixth access port **232** may serve one or more of a variety of functions as well including withdrawal of sample after final detection. Optionally, as with fifth access port **230**, sixth access port **232** may be attached to a fluid reservoir compartment. In addition, sixth access port **232** may interface additional laser ablated microstructures for communicating a sample droplet to a post-column collection device (see Figures 17 and 18).

[0151] Figure 16 illustrates a μ -TAS **250** having a laser-ablated fluid reservoir compartment **252** as an integral "on-device" microstructure on the substrate. Fluid reservoir compartment **252** may be formed by laser ablation of a suitable microstructure in the substrate to provide a compartment in which buffers or other reagents may be held. Such reservoir compartment may be used to provide a makeup flow fluid, a flow regulation function or to provide a reagent for post-separation pre-detection analyte derivatization.

[0152] In one example depicted in Figure 16A, reservoir microstructure **252** having inlet port **254** and outlet port **256** is laser ablated into planar substrate **258**. The reservoir microstructure may be formed in any geometry and with any aspect ratio to provide a reservoir compartment having a desired volume. Outlet port **256** can be in fluid communication with sample processing compartment **260** by way of interconnecting microchannel **262**. The inlet port is optionally divertably connected to an external source of fluid from which the reservoir compartment may be filled. The reservoir compartment **252**, interconnecting reservoir flow component **262**, and sample processing compartment **260** are respectively formed from the reservoir microstructure and the interconnecting, microchannel in combination with cover plate **264**.

[0153] In another example illustrated in Figure 16B, fluid reservoir compartment **252** may be formed by laser ablating a reservoir microstructure **252** having an inlet port **254** and an outlet port **256** into first planar substrate **258** and mirror image structures **252'**, **254'** and **256'** in second planar substrate **258'**. The reservoir compartment **252** is formed when the first and second substrates

are aligned as described in detail above.

[0154] Buffers or reagents held in the fluid reservoir compartment may be delivered to sample processing compartment **260**, to a sample flow component or to a sample treatment component reservoir compartment **252** via connecting microchannel **262**. Fluid flow from the reservoir compartment to the sample processing compartment may occur via passive diffusion. Optionally, the fluid may be displaced from the reservoir compartment by an actuator means. A variety of micropumps and microvalves that will find utility as an actuator means according to the invention disclosed herein are well known in the art and have been described, for example, in Manz et al. (1993) *Adv. Chromatogr.* **33**:1-66 and references cited therein.

[0155] As illustrated in cross-section in Figure 16C, the reservoir compartment **252** is optionally covered with thin membrane **266** to form a diaphragm-type pump; passive one-way microvalve **268** is optionally integrated into interconnecting microchannel **262** to prevent backflow of displaced fluid into the reservoir compartment. Optional gas- or liquid-filled cavity **270** is disposed above the membrane. Actuator means **272** can be employed to effect fluid displacement from reservoir compartment **252** by deflection of membrane **266**.

[0156] Actuator means **272** may act to directly deflect membrane **266**. Accordingly, the actuator means may be a piezoelectric, piston, solenoid or other type of membrane-deflecting device. Alternatively, the actuator means can be a heating means by which the temperature inside cavity **270** can be regulated. The heating means may be a resistance-type heating means or any type of suitable heating means known in the art. Upon actuation, the temperature of the heating means increases, thereby heating the contents of cavity **270** and increasing the volume thereof, producing a downward deflection of membrane **266**, and displacing fluid from reservoir compartment **252**, into interconnecting microchannel **262**, past valve **268** and into sample processing compartment **260**.

[0157] Alternatively, heating means **272** may be disposed in thermal contact with reservoir compartment **252** itself. In this configuration, as the heating means temperature increases, the volume of the fluid in the reservoir compartment increases and is thereby displaced from the reservoir compartment into the sample processing compartment.

[0158] Other examples of pumping mechanisms which may be incorporated into the μ -TAS disclosed and claimed herein include those which operate on the principles of ultrasonic-induced transport (Moroney et al. (1991) *Proc MEM S'91*, p. 277) or electrohydrodynamic-induced transport (Richter et al. (1991) *Proc MEM S'91* p. 271). In addition, chemical valves composed of electrically driven polyelectrolyte gels (Osada (1991) *Adv. Materials* **3**:107; Osada et al. (1992) *Nature* **355**:242) may be used.

[0159] Microstructures laser ablated in the substrate

for communicating a sample droplet to a post-column sample collection device (320) are generally shown in Figure 17. Figures 17A, 17B and 17C are cross-sections of a μ -TAS illustrating means whereby sample droplets are generated and expelled from the μ -TAS for post-column collection. Referring now to Figure 17A, sixth sample flow component 212 and sixth access port 232 are in fluid communication with sample delivery means 302 comprising mixing chamber 304 in fluid communication and in axial alignment with sixth access port 232, fluid communication means 306 and an outlet nozzle 308. The fluid communication means 306 may be a conduit interfaced with an external source of fluid (Figure 17A) or a microchannel (Figure 17C) laser ablated in the substrate. As shown in Figure 17A, fluid communication means 306 is in divertable fluid communication with an external reservoir of gas or liquid (not shown) and a means whereby a pulse of gas or liquid may be expelled from the external reservoir, thereby generating sample droplet 310. In Figure 17A, post-column collection device 320 shown therein in cross-section may be a substrate in which sample droplet receiving microwell 322 has been laser ablated. As described with respect to other microstructures formed by laser ablation, microwell 322 may be of any geometry and any aspect ratio. Post-column collection device 320 is shown in greater detail in Figure 18.

[0160] A further example of means for generating and expelling a sample droplet from a μ -TAS is shown in cross-section in Figure 17B. A heating means 312 can be situated in thermal contact with sample delivery means 302. As the temperature of heating means 312 increases, a steam bubble builds up in mixing chamber 304, thereby forming sample droplet 310. For further discussion of fluid delivery using this method see Allen et al. (1985) *Hewlett-Packard J. May 1985*:21-27. As in Figure 17A, post-column collection device 320 shown in Figure 17B in cross-section may be a substrate in which sample droplet receiving microwell 322 has been laser ablated. In addition, cover plate 324 may be movably interposed between the μ -TAS and the post-column collection device 320. Cover plate 324 is a structure that has an opening 326 in axial alignment with nozzle 308 and receiving well 322 and is intended to provide protection of empty or filled wells from contamination or from evaporation of sample droplets previously collected.

[0161] Yet another example of means for generating and expelling a sample droplet from a μ -TAS is shown in cross-section in Figure 17C. As illustrated in Figure 17C, and in further reference to Figure 16, fluid communication means 306 can be interconnecting microchannel 262 having a first end in fluid communication with sixth access port 232 and a second end in fluid communication with on-device fluid reservoir compartment 252. Alternatively, fluid communication means 306 may be a microchannel having a first end in fluid communication with sixth access port 232 and a second end

terminating in an access port which is in fluid communication with an external fluid reservoir (not shown). Heating means 312 may be situated in thermal contact with fluid communication means 306. As described above, actuation of heating means 312 results in the increase in the temperature thereof, the build up of a steam bubble in mixing chamber 304, and the formation and expulsion of sample droplet 310. Fluid communication means 306 is optionally formed from a microchannel laser ablated in cover plate 264 or from mirror-image microchannels laser ablated in interior surfaces 258 and 258'. As in Figures 17A and 17B, post-column collection device 320 shown in Figure 17C in cross-section may be a substrate which holds a bibulous sheet means 328 for solid phase sample collection. Bibulous sheet means 328 for solid-phase sample collection may be filter paper, absorbent membranes, or the like. As described with respect to Figure 17B, cover plate 324 may optionally be movably interposed between the μ -TAS and the post-column collection device 320.

[0162] As shown in Figure 18, post-column collection device 320 comprising sample receiving means that may be sample receiving wells 322 or bibulous sheet means 328 can be positioned relative to nozzle means 308 to receive the sample droplet 310 from the nozzle means. The sample receiving means may be a microwell 322 laser ablated in a substrate for liquid phase sample collection or may be a bibulous sheet means 328 for solid-phase sample collection. The substrate for post-column collection device 320 is optionally a material other than silicon or silicon dioxide and microwells 322 are laser-ablated in the substrate. As shown in Figure 18, the receiving means is optionally in rotatable alignment with the outlet nozzle such that multiple fractions may be collected. Alternatively, as shown in Figure 18B, post-column collection device 320 includes protection means 324 with opening 326 in axial alignment with the outlet nozzle, wherein protection means 324 is interposed between μ -TAS 200 and sample receiving wells 322. Although post-column collection device 320 is depicted as a disc in rotatable alignment with μ -TAS 200, it will be recognized by one of skill in the art that the configuration of the collection device need not be so limited. Thus, post-column collection device 320 may be configured, for example, as a linear arrangement of sample receiving wells 322, or the like.

[0163] It is to be understood that, while the invention has been described in conjunction with the preferred specific embodiments thereof, the description above as well as the example which follows are intended to illustrate and not limit the scope of the invention. Other aspects, advantages and modifications within the scope of the invention will be apparent to those skilled in the art to which the invention pertains.

[0164] The following example is put forth so as to provide those of ordinary skill in the art with a complete disclosure and description of how to use the method of the invention, and is not intended to limit the scope of what

the inventors regard as their invention. Efforts have been made to ensure accuracy with respect to numbers (e.g., amounts, temperature, etc.) but some errors and deviations should be accounted for. Unless indicated otherwise, parts are parts by weight, temperature is in °C and pressure is at or near atmospheric.

Example 1

Separation of Immunoglobulins from Serum

[0165] The serum sample used in this Example is composed of the following immunoglobulin analytes.

	IgG	IgA	IgM
Concentration (mg/dl)	1200	200	100
μ	γ	fast γ to β	fast γ to β
Mass (kDa)	150	160	900

[0166] Examples of other serum constituents from which the immunoglobulin analytes will be extracted include albumin (4600 mg/dl), bilirubin (0.4 mg/dl), cholesterol (211 mg/dl), creatinine (1.1 mg/dl), glucose (108 mg/dl), calcium (9.8 mg/dl), phosphorous (4.0 mg/dl), nitrogen as urea (15 mg/dl) and uric acid (5.9 mg/dl).

[0167] A μ -TAS device with exterior dimensions of approximately 20 mm x 60 mm is fabricated using the laser ablation techniques described above in a polyimide material available under the trademark Kapton® from DuPont (Wilmington, Delaware). Unless otherwise noted, the dimensions of the sample treatment components in millimeters are indicated below as width x length x depth.

[0168] First sample treatment component 214 is approximately 5 x 10 x 0.2. This provides component with a volume of 2.0 μ l. The component is loaded with a matrix having a high surface area, for example, a microparticle or a membrane material, and having specificity for the analyte, in this case immunoglobulins G, A or M. The specificity of the analyte-matrix interaction is based on, for example, the hydrophobic nature of the analyte (e.g., reverse phase or hydrophobic interaction chromatography) or the ionic character of the analyte (e.g., ion exchange chromatography). On the other hand, the specificity may be based on the specific affinity of the matrix for the analyte. In either case, the function of the first sample treatment component is to "capture" the desired analyte and thereby provide a preconcentration function. First and second access ports 222 and 224 are laser ablated in the substrate and provide means by which fluids may be introduced into or withdrawn from first and second sample flow components 202 and 204 which flank first sample treatment component 214 and which are in fluid communication therewith. First and second access ports 222 and 224 are in divertable com-

munication with a valving manifold such that valves specifically associated with the indicated ports can be individually "actuated" to isolate this component during the "capture" step. In this manner, undesirable constituents in the samples are flushed to waste during sample loading and prior to elution of the analyte from the first sample treatment component.

[0169] For the purpose of the example, 5 μ l of human serum, containing a total of about 150 femtomoles of IgG, 2.2 femtomoles of IgM and 25 femtomoles of IgA, is loaded onto first sample treatment component 214, which contains a membrane material containing protein A/G (Pierce) which binds to IgG, IgA and IgM. Sample loading may be done by injecting a bolus thereof or pumping the sample into the component through first access port 222. The sample is allowed to equilibrate with the protein in the first sample treatment component 214. The component is then flushed with a buffer solution to clear the chamber of other unbound solutes in the sample.

[0170] After the sample has equilibrated with the capture matrix in the first sample treatment component 214, valves associated with first and second access ports 222 and 224 are actuated, and a decoupling solution pumped through the component to elute the analyte from the matrix. A qualitative spectrophotometer optically coupled to first detection means 234 is monitored to determine when the analyte has been eluted from first sample treatment component 214 and has been loaded on the second sample treatment component 216.

[0171] Second sample treatment component 216 (3 x 30 x 0.2; 18 μ l) is designed to serve a desalting function. There are several modes which may be used to desalt the analyte. For example, desalting can be accomplished using an electromotive separation based on the different mobilities of small and large solutes in a particular matrix. One alternative desalting method uses fluid pressure as a means for effecting mass transport, with size exclusion chromatography as the mode of separation. Further, it is possible that a mode combining both motive forces could be applied simultaneously, using an electrochromatography separation mode (see, e.g., Knox et al. (1987) *Chromatographia* 24:135; Knox et al. (1989) *J. Liq. Chromatogr* 12:2435; Knox et al. (1991) *Chromatographia* 32:317).

[0172] For the purpose of this example, second sample treatment component 216 contains an anti-convective media such as polyacrylamide, polymethylmethacrylate or agarose. Valves associated with second and third access ports 224 and 226 are actuated to isolate the second sample treatment component 216 during this step.

[0173] Third sample treatment component 218 (3 x 40 x 0.2; 24 μ l) serves an analyte band focusing function. After the capture and desalting steps, it is likely that band broadening will have occurred, and so a band focusing step is required. Analyte focusing can be done either by isoelectric focusing (IEF) mechanism in a gel

matrix, chromatofocusing, or by isotachopheresis.

[0174] For the purpose of this example, third sample treatment component 218 contains a liquid ampholyte or an ampholyte in a gel matrix as described by Wehr et al (1990) *Am. Biotechnol. Lab.* 8:22 and Kilar et al. (1989) *Electrophoresis* 10:23-29.

[0175] Valves coupled to third and fourth access ports 226 and 228 are actuated in order to equilibrate the matrix in third sample treatment component 218 with the appropriate buffer. Valves communicating with second and fourth access ports 224 and 228 are then actuated to elute the analyte from second sample treatment component 216. Second detection means 236 is monitored to determine when all of the analyte has been loaded into third sample treatment component 218. Finally, the pH gradient is produced by actuating valves communicating with third and fourth access ports 226 and 228. A so-called polybuffer having an operating range of pH 7-4 or 9-6 (Sigma) is used. Separation of IgG from IgM and IgA occurs in this step.

[0176] Fourth sample treatment component 220 (50 µm x 50 mm; 100 nl) effects the final separation of IgA from IgM. The separation is accomplished using capillary zone electrophoresis (CZE), in which the separation of IgA and IgM occurs based on the large difference between the charge/size ratio. As above, this component is loaded and isolated by actuation of valves in the manifold which communicate with fourth and fifth access ports 228 and 230 and sample loading is monitored via third detection means 238.

[0177] The last step of the exemplary determination of serum immunoglobulin analytes by the µ-TAS occurs in fifth sample flow component 210 by monitoring fourth detection means 240. This is the detection on which analyte quantitation is based. Spectrophotometric detection would provide the quantitative data required. Fifth access port 230 is used as a means for introducing a reagent for post-column derivatization, e.g., dansylation or dabsylation, and detection. Femtomoles of immunoglobulins in nanoliters of final elution buffer yield micromolar to high nanomolar concentrations. Depending on the path length and mode of spectrophotometric detection, no reagent may be needed.

Claims

1. A miniaturized column device (2) for use in a liquid phase analysis system, said miniaturized column device (102) comprising:

(a) a support body (104) formed from a substrate comprised of a laser-ablatable material, said support body (104) having first (106) and second (108) component halves each having substantially planar interior surfaces (110, 112);
(b) a first microchannel (114) laser-ablated in the interior surface (110) of the first support

body half (104) and a second microchannel (116) laser-ablated in the interior surface (112) of the second support body half (108), wherein said first (114) and second (116) microchannels are arranged so as to provide the mirror image of the other;

(c) a sample processing compartment (118) formed by aligning the interior surfaces (110, 112) of the support body halves (106, 108) in facing abutment with each other whereby the microchannels (114, 116) define said sample processing compartment (118) and wherein said sample processing compartment (118) comprises sample handling regions (202, 204, 206, 208, 210, 212, 214, 216, 218, 220) which define a sample flow component (202, 204, 206, 208, 210, 212) in fluid communication with a sample treatment component (214, 216, 218, 220); and

(d) at least one inlet port (120) and at least one outlet port (124) communicating with the sample processing compartment (118), said ports enabling the passage of fluid from an external source through the sample processing compartment (118).

2. The miniaturized column device of claim 1, wherein the sample processing compartment (118) comprises a serial arrangement of sample handling regions (202, 204, 206, 208, 210, 212, 214, 216, 218, 220) which define a serial arrangement of alternating sample flow components (202, 204, 206, 208, 210, 212) and sample treatment components (214, 216, 218, 220).
3. The miniaturized column device of claim 2, further comprising detection means (232, 234, 236, 238, 240) laser-ablated in the substrate, wherein said detection means (232, 234, 236, 238, 240) is in communication with the sample processing compartment (118) thereby enabling the detection of a sample passing through the sample processing compartment (118).

Patentansprüche

1. Ein miniaturisiertes Säulenbauelement (2) zur Verwendung bei einem Flüssigphasenanalysesystem, wobei das miniaturisierte Säulenbauelement folgende Merkmale aufweist:

(a) einen Trägerkörper (104), der aus einem Substrat gebildet ist, das ein laserablatierbares Material aufweist, wobei der Trägerkörper (104) eine erste (106) und eine zweite (108) Komponentenhälfte aufweist, die jeweils im wesentlichen planare Innenoberflächen (110,

112) aufweisen;

(b) einen ersten Mikrokanal (114), der in die Innenoberfläche (110) der ersten Trägerkörperhälfte (104) laserablatiert ist, und einen zweiten Mikrokanal (116), der in die Innenoberfläche (112) der zweiten Trägerkörperhälfte (108) laserablatiert ist, wobei der erste (114) und zweite (116) Mikrokanal angeordnet sind, um das Spiegelbild des anderen bereitzustellen;

(c) ein Probenverarbeitungsfach (118), das durch Ausrichten der Innenoberflächen (110, 112) der Trägerkörperhälften (106, 108) aneinander anstoßend gebildet ist, wodurch die Mikrokanäle (114, 116) das Probenverarbeitungsfach (118) definieren und wobei das Probenverarbeitungsfach (118) Probenhandhabungsregionen (202, 204, 206, 208, 210, 212, 214, 216, 218, 220) aufweist, die eine Probenflußkomponente (202, 204, 206, 208, 210, 212) in Fluidkommunikation mit einer Probenbehandlungskomponente (214, 216, 218, 220) definieren; und

(d) zumindest eine Einlaßöffnung (120) und zumindest eine Auslaßöffnung (124), die mit dem Probenverarbeitungsfach (118) kommunizieren, wobei die Öffnungen ermöglichen, daß ein Fluid aus einer externen Quelle das Probenverarbeitungsfach (118) passiert.

2. Das miniaturisierte Säulenbauelement gemäß Anspruch 1, bei dem das Probenverarbeitungsfach (118) eine serielle Anordnung von Probenhandhabungsregionen (202, 204, 206, 208, 210, 212, 214, 216, 218, 220) aufweist, die eine serielle Anordnung alternierender Probenflußkomponenten (202, 204, 206, 208, 210, 212) und Probenbehandlungskomponenten (214, 216, 218, 220) definieren.

3. Das miniaturisierte Säulenbauelement gemäß Anspruch 2, das ferner eine Erfassungseinrichtung (232, 234, 236, 238, 240) aufweist, die in das Substrat laserablatiert ist, wobei die Erfassungseinrichtung (232, 234, 236, 238, 240) in Kommunikation mit dem Probenverarbeitungsfach (118) steht, wodurch sie die Erfassung einer Probe, die das Probenverarbeitungsfach (118) passiert, ermöglicht.

Revendications

1. Dispositif de colonne miniaturisé (2) destiné à être utilisé dans un système d'analyse en phase liquide, ledit dispositif de colonne miniaturisé (102) comprenant :

(a) un corps de support (104) formé à partir d'un substrat composé d'un matériau pouvant être ablaté au laser, ledit corps de support (104) ayant des première (106) et seconde (108) moitiés de composant ayant chacune des surfaces intérieures sensiblement planes (110, 112) ;

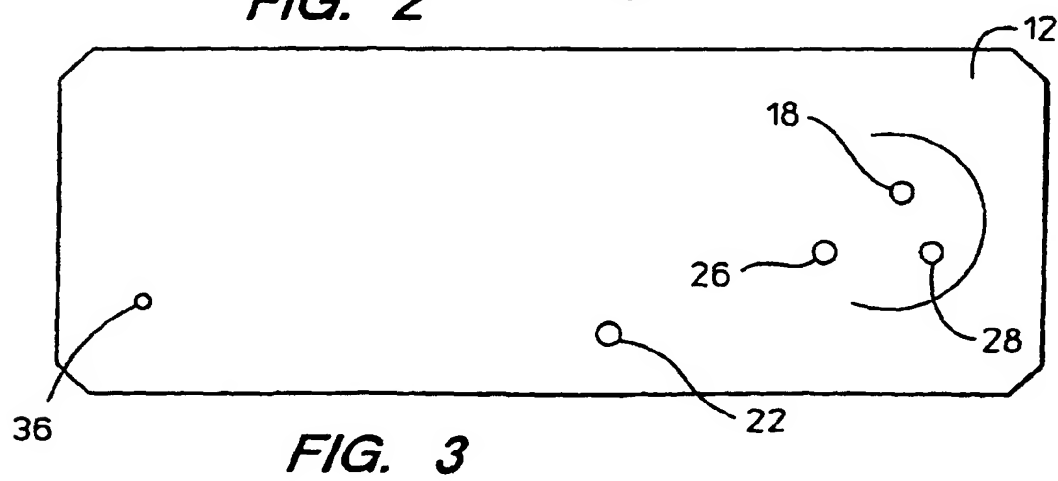
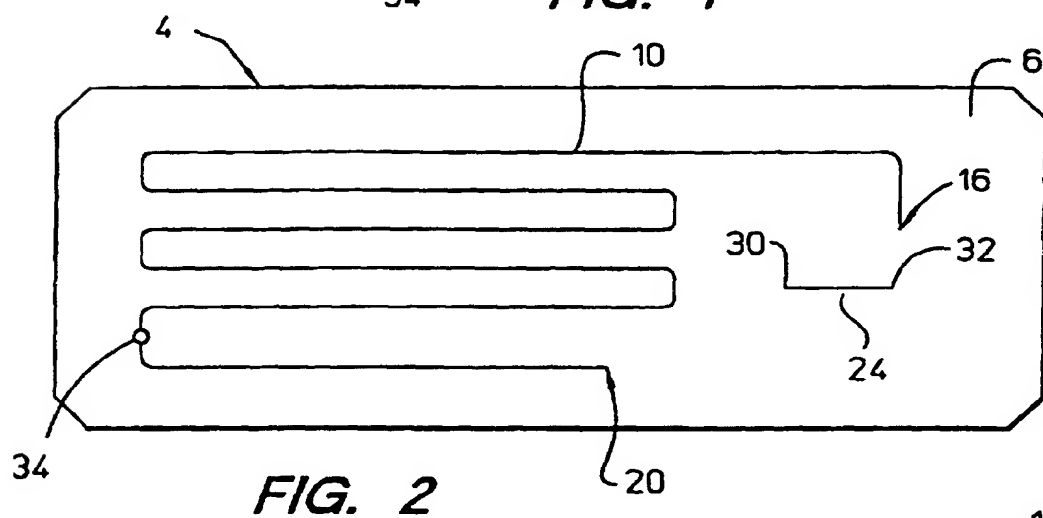
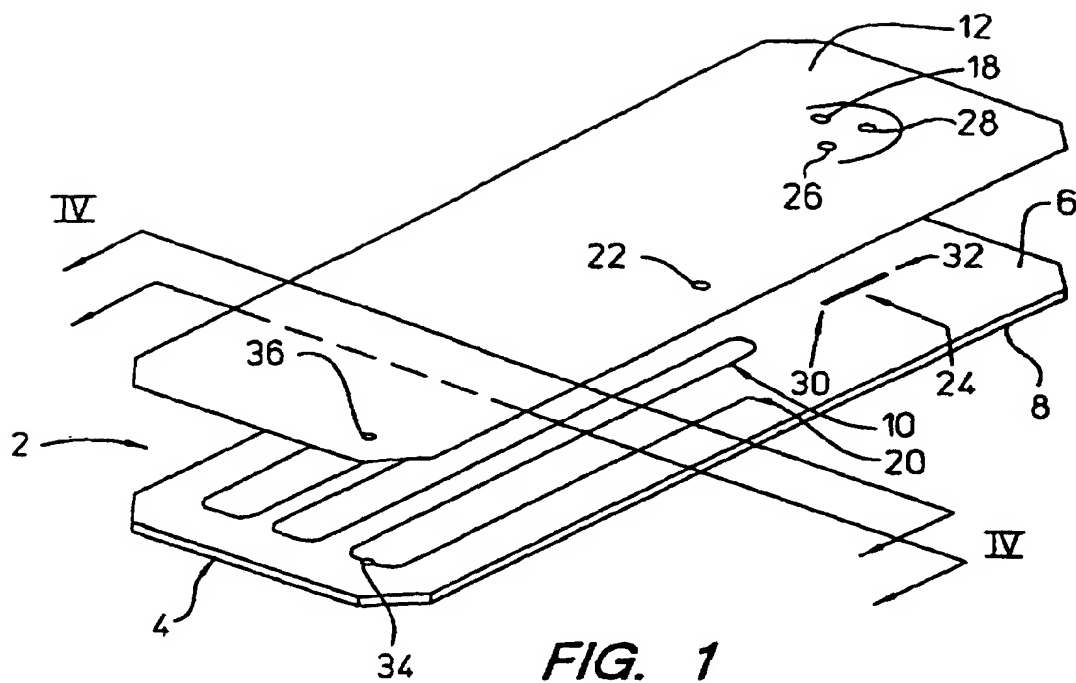
(b) un premier micro-canal (114) ablaté au laser dans la surface intérieure (110) de la première moitié de corps de support (104) et un second micro-canal (116) ablaté au laser dans la surface intérieure (112) de la seconde moitié de corps de support (108), dans lequel lesdits premier (114) et second (116) micro-canaux sont disposés de manière à fournir l'image inverse de l'autre ;

(c) un compartiment de traitement d'échantillon (118) formé en alignant les surfaces intérieures (110, 112) des moitiés de corps de support (106, 108) en butée opposée l'une par rapport à l'autre, moyennant quoi les micro-canaux (114, 116) définissent ledit compartiment de traitement d'échantillon (118) et dans lequel ledit compartiment de traitement d'échantillon (118) comprend des zones de manipulation d'échantillon (202, 204, 206, 208, 210, 212, 214, 216, 218, 220) qui définissent un composant d'écoulement d'échantillon (202, 204, 206, 208, 210, 212) en communication fluidique avec un composant de traitement d'échantillon (214, 216, 218, 220) ; et

(d) au moins un orifice d'entrée (120) et au moins un orifice de sortie (124) communiquant avec le compartiment de traitement d'échantillon (118), lesdits orifices permettant le passage de fluide depuis une source externe à travers le compartiment de traitement d'échantillon (118).

2. Dispositif de colonne miniaturisé selon la revendication 1, dans lequel le compartiment de traitement d'échantillon (118) comprend un agencement en série de zones de manipulation d'échantillon (202, 204, 206, 208, 210, 212, 214, 216, 218, 220) qui définissent un agencement en série de composants d'écoulement d'échantillon alternés (202, 204, 206, 208, 210, 212) et de composants de traitement d'échantillon (214, 216, 218, 220).

3. Dispositif de colonne miniaturisé selon la revendication 2, comprenant en outre des moyens de détection (232, 234, 236, 238, 240) ablatés au laser dans le substrat, dans lequel lesdits moyens de détection (232, 234, 236, 238, 240) sont en communication avec le compartiment de traitement d'échantillon (118) pour permettre ainsi la détection d'un échantillon passant à travers le compartiment de traitement d'échantillon (118).



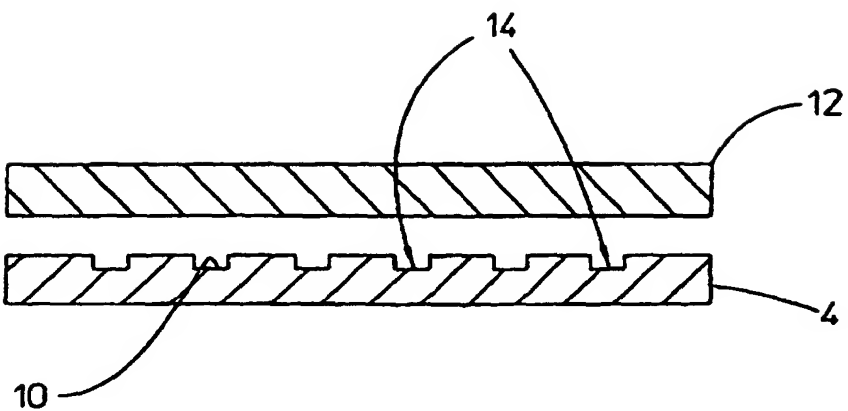


FIG. 4

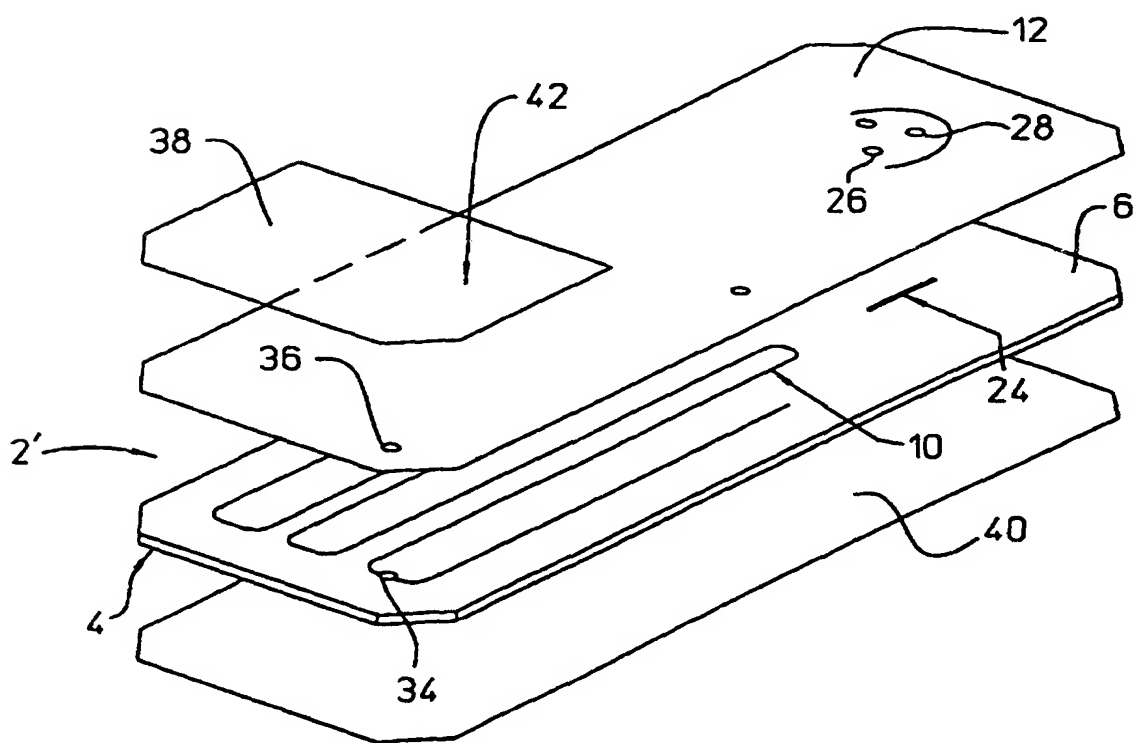


FIG. 5

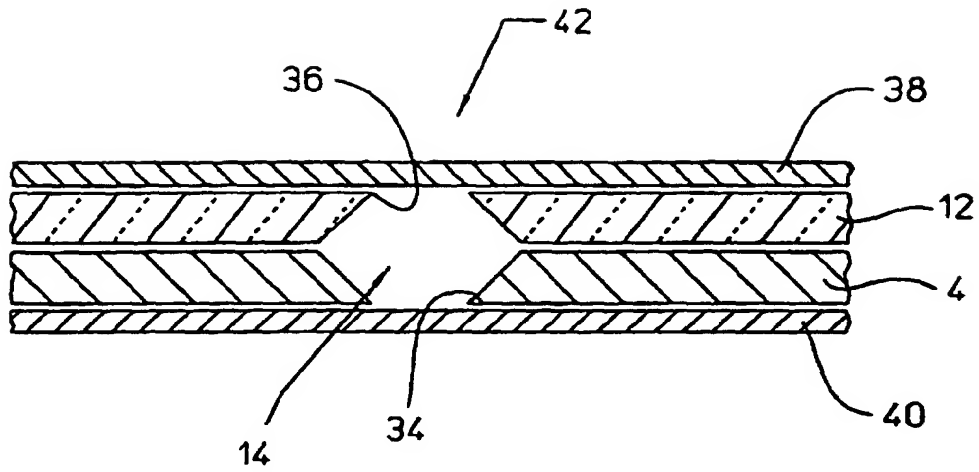


FIG. 6

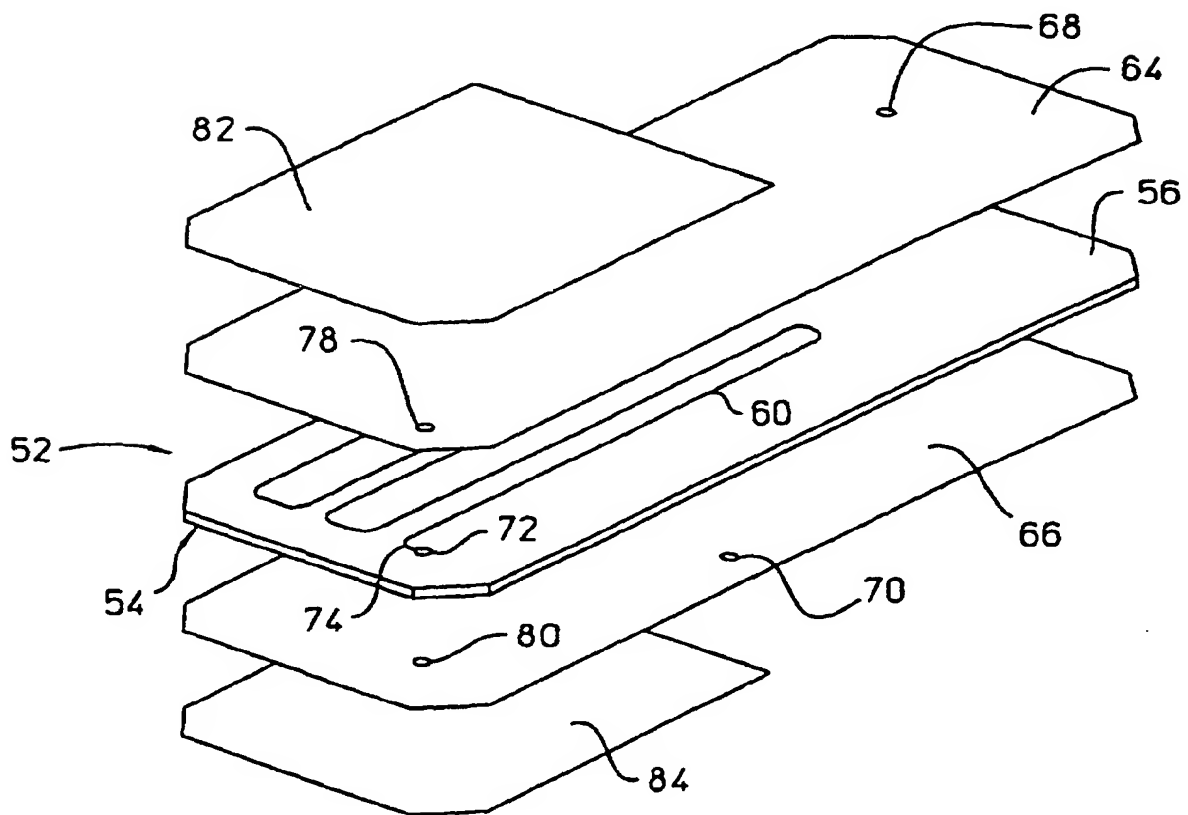


FIG. 7A

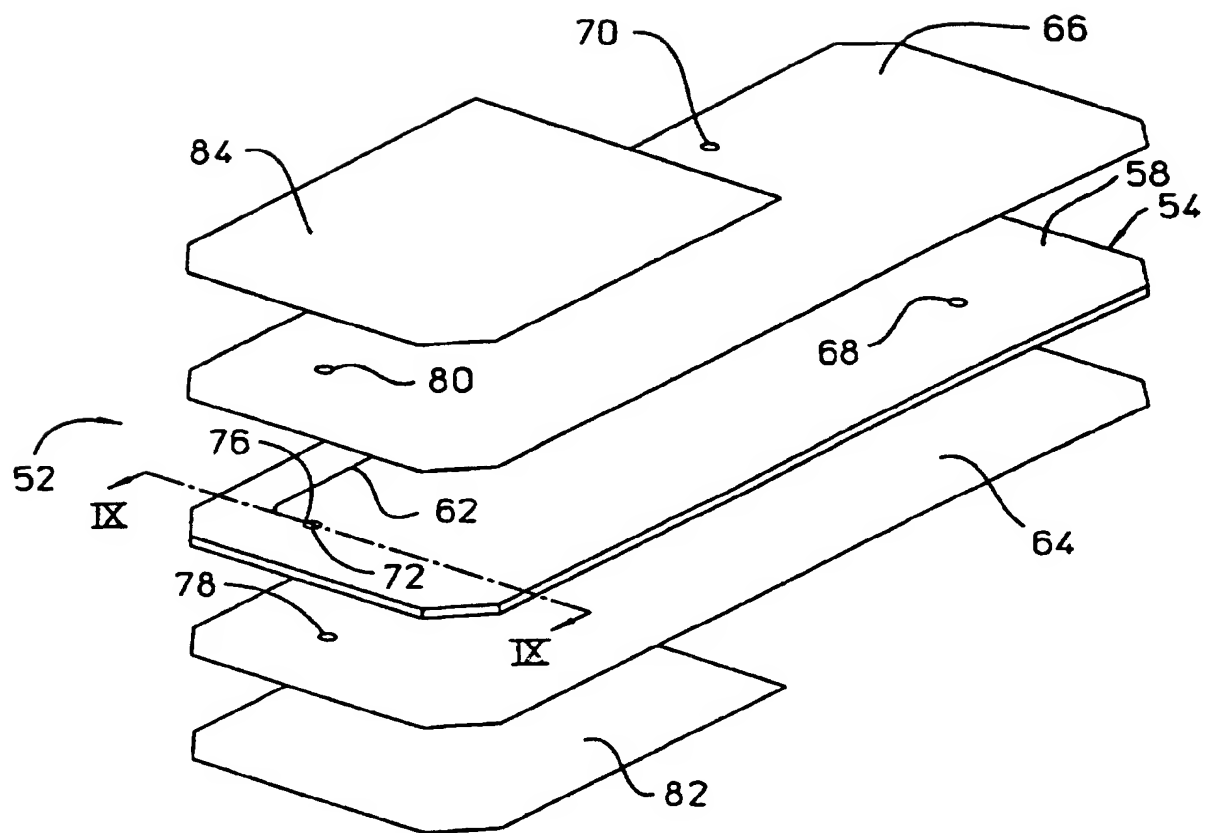


FIG. 7B

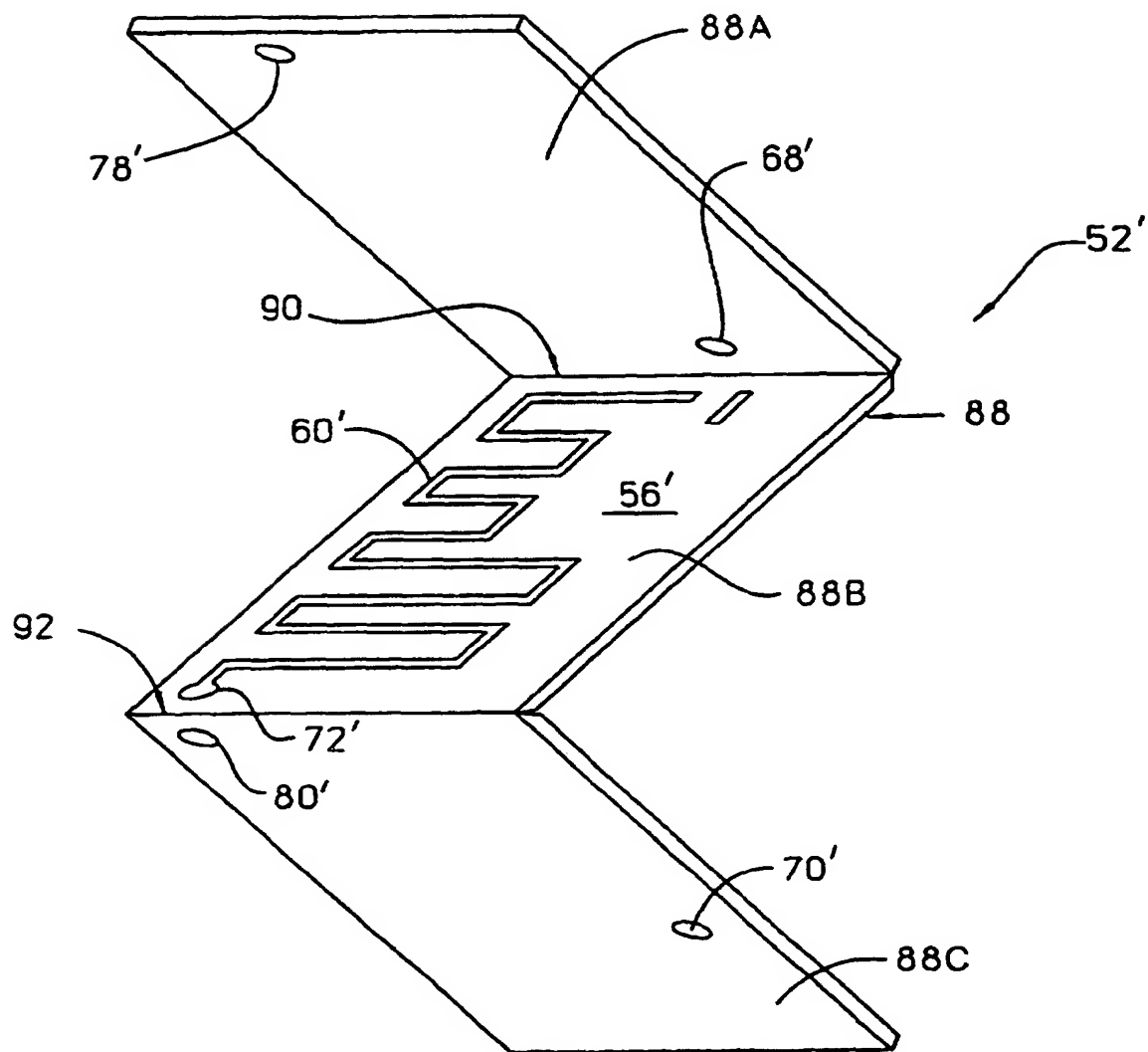


FIG. 8A

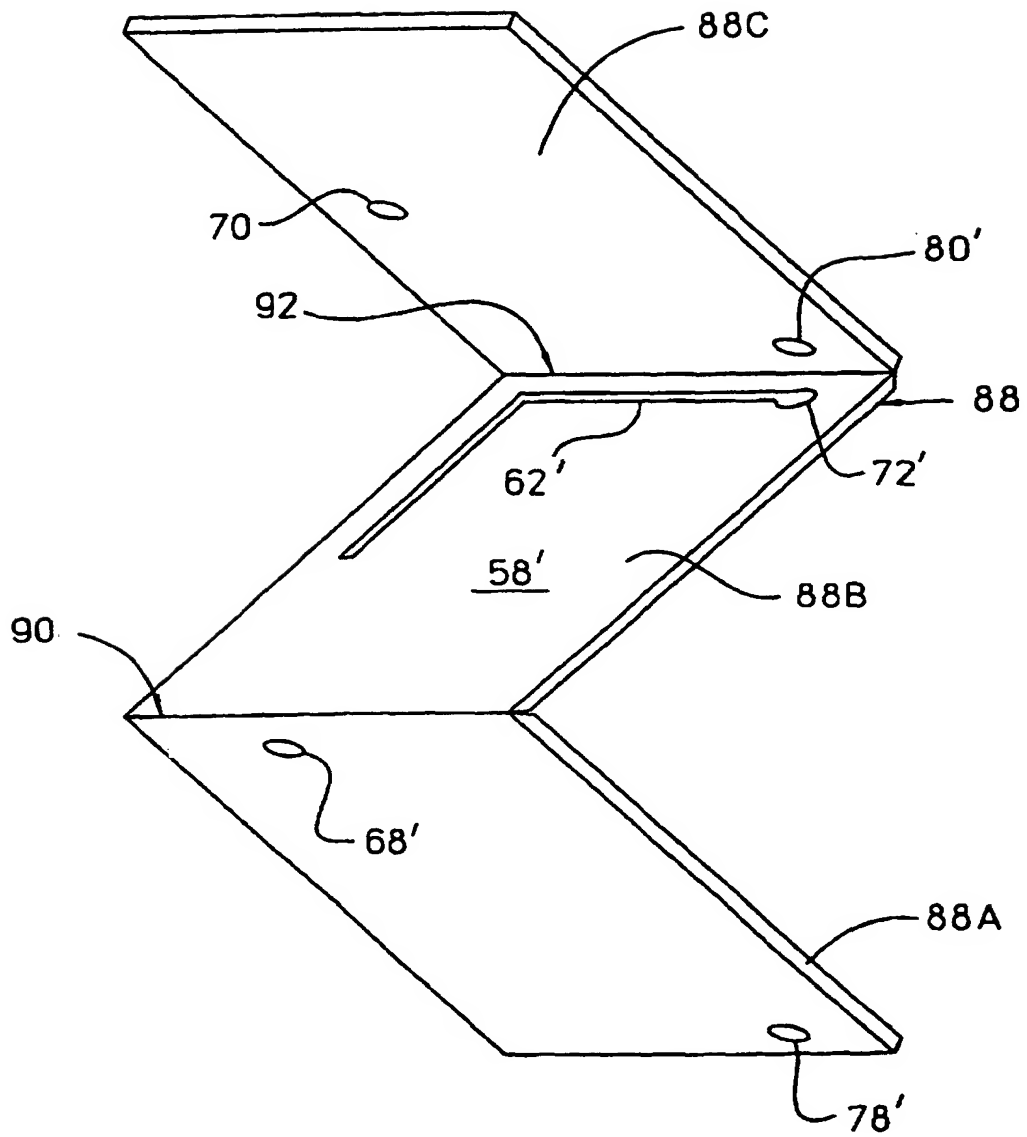


FIG. 8B

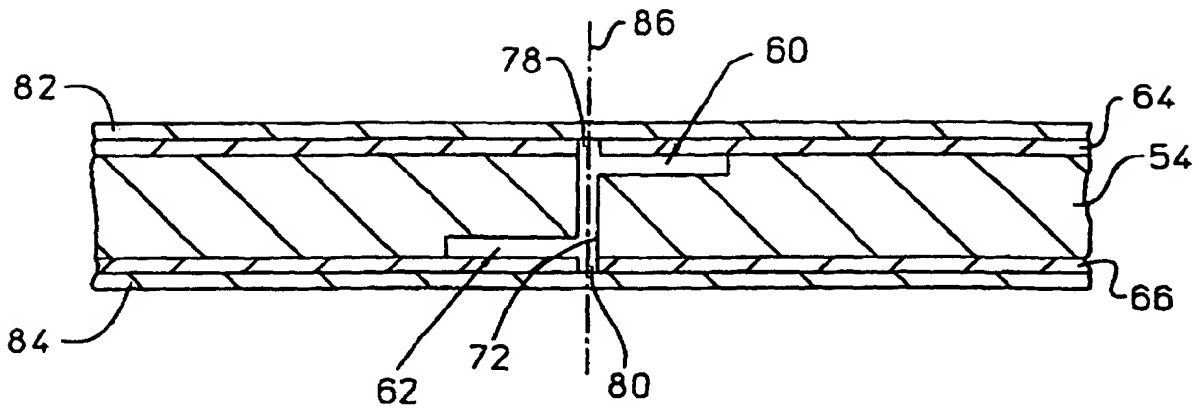


FIG. 9

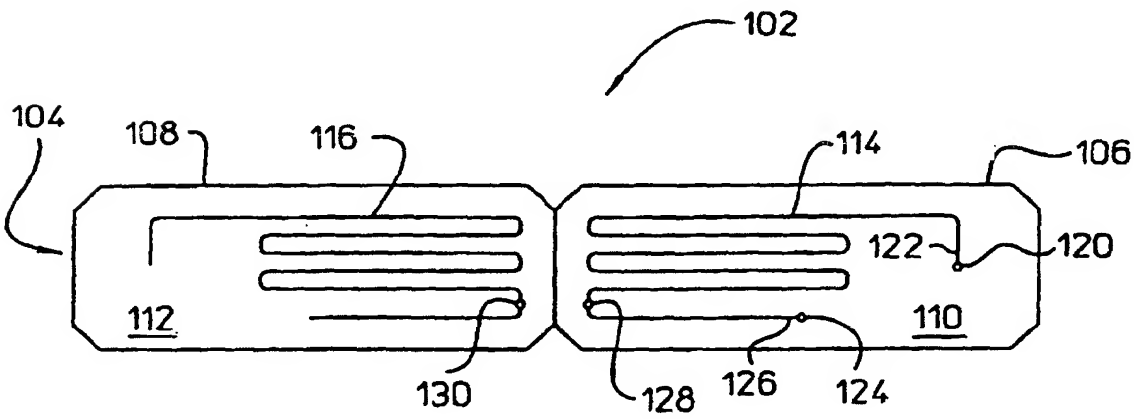


FIG. 10

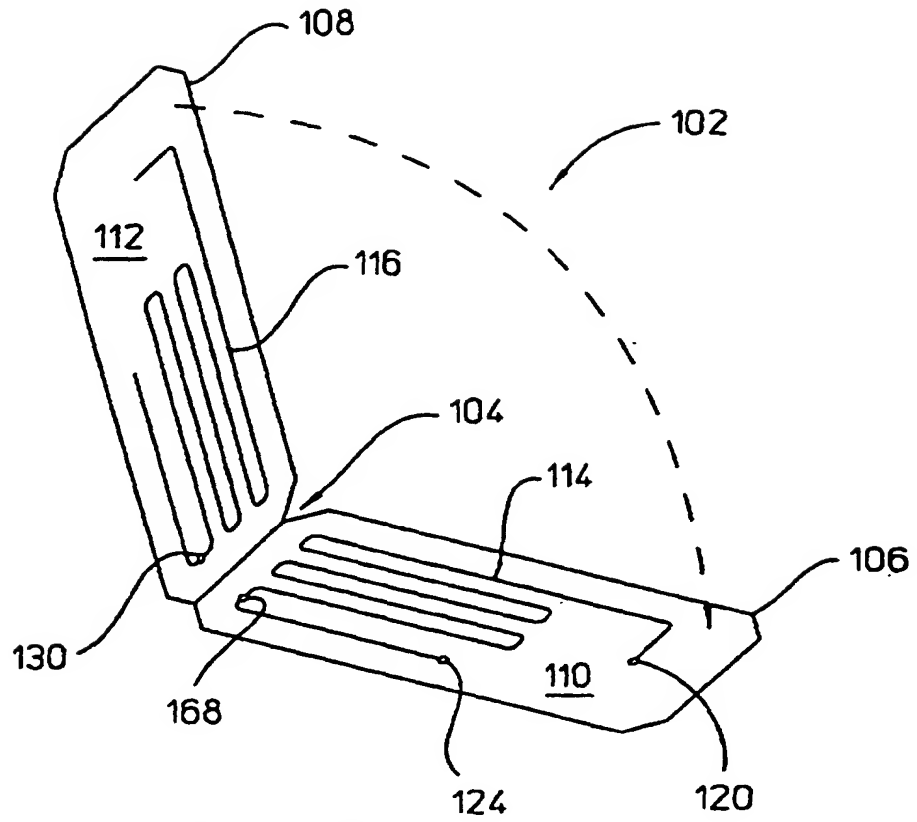


FIG. 11

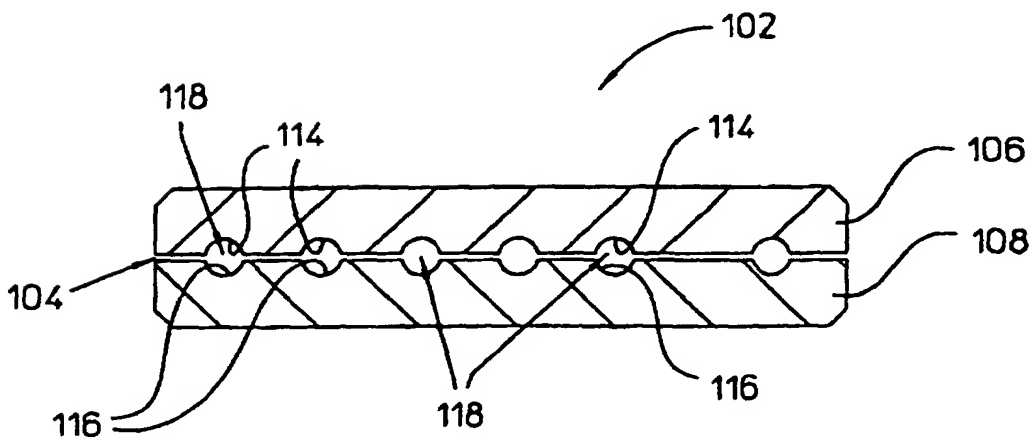


FIG. 12

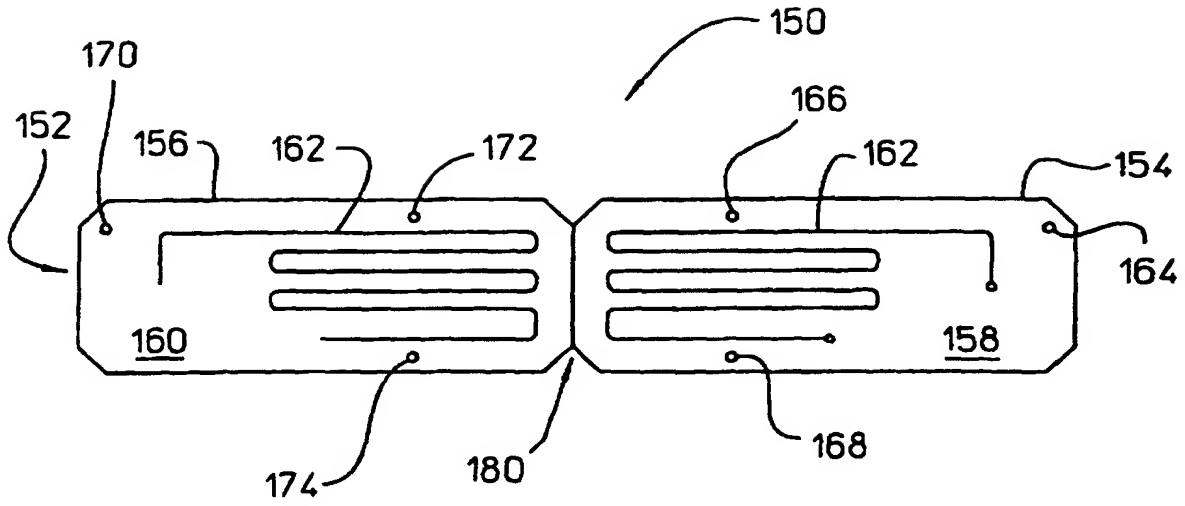


FIG. 13

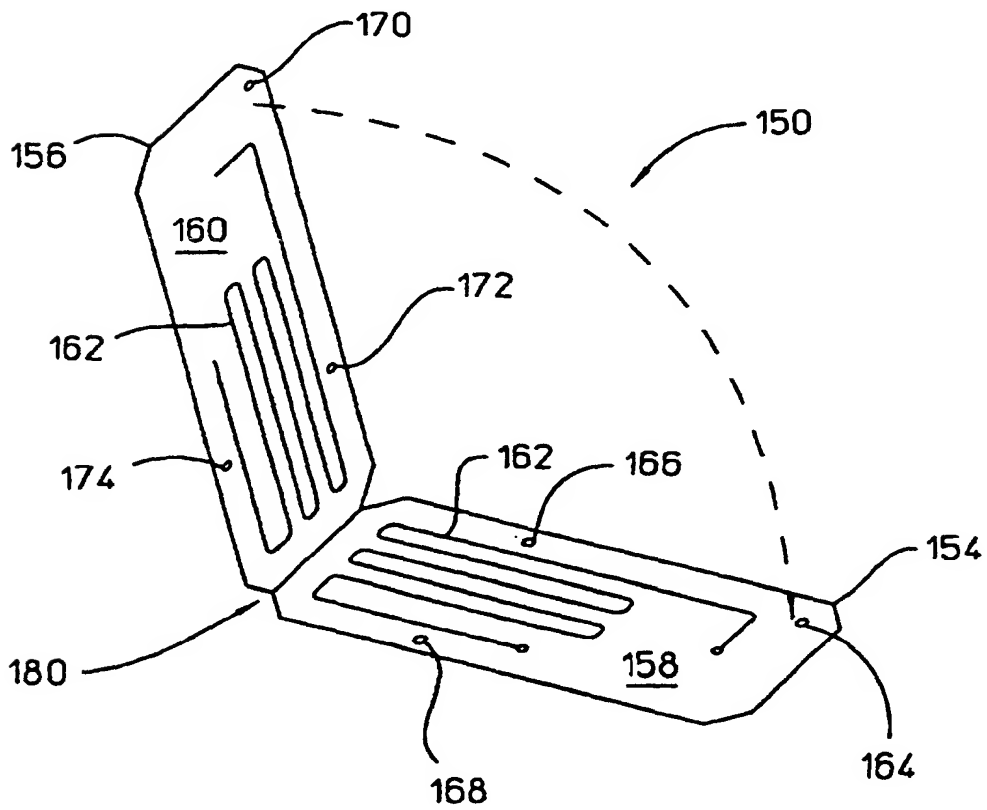


FIG. 14

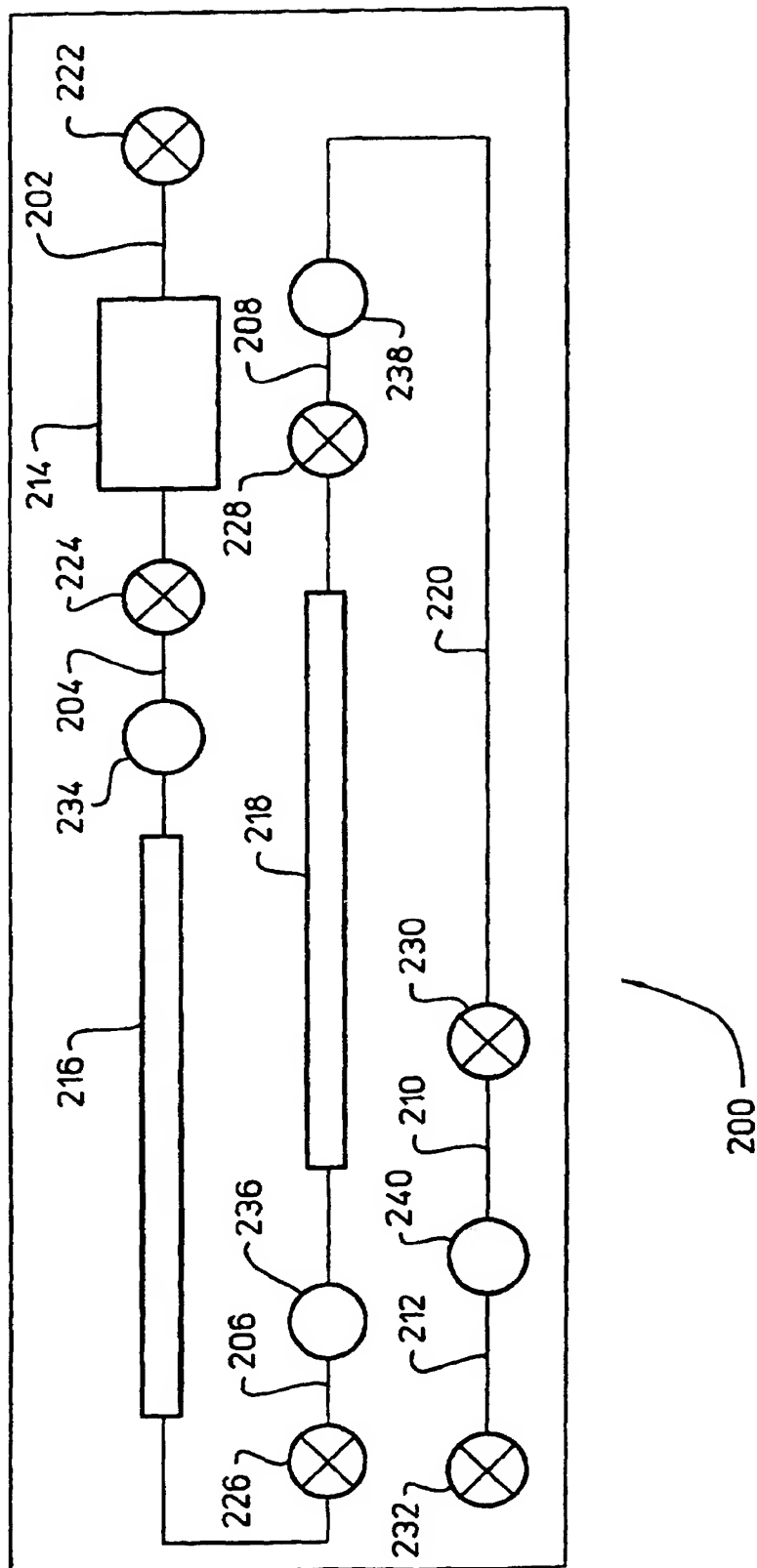


FIG. 15

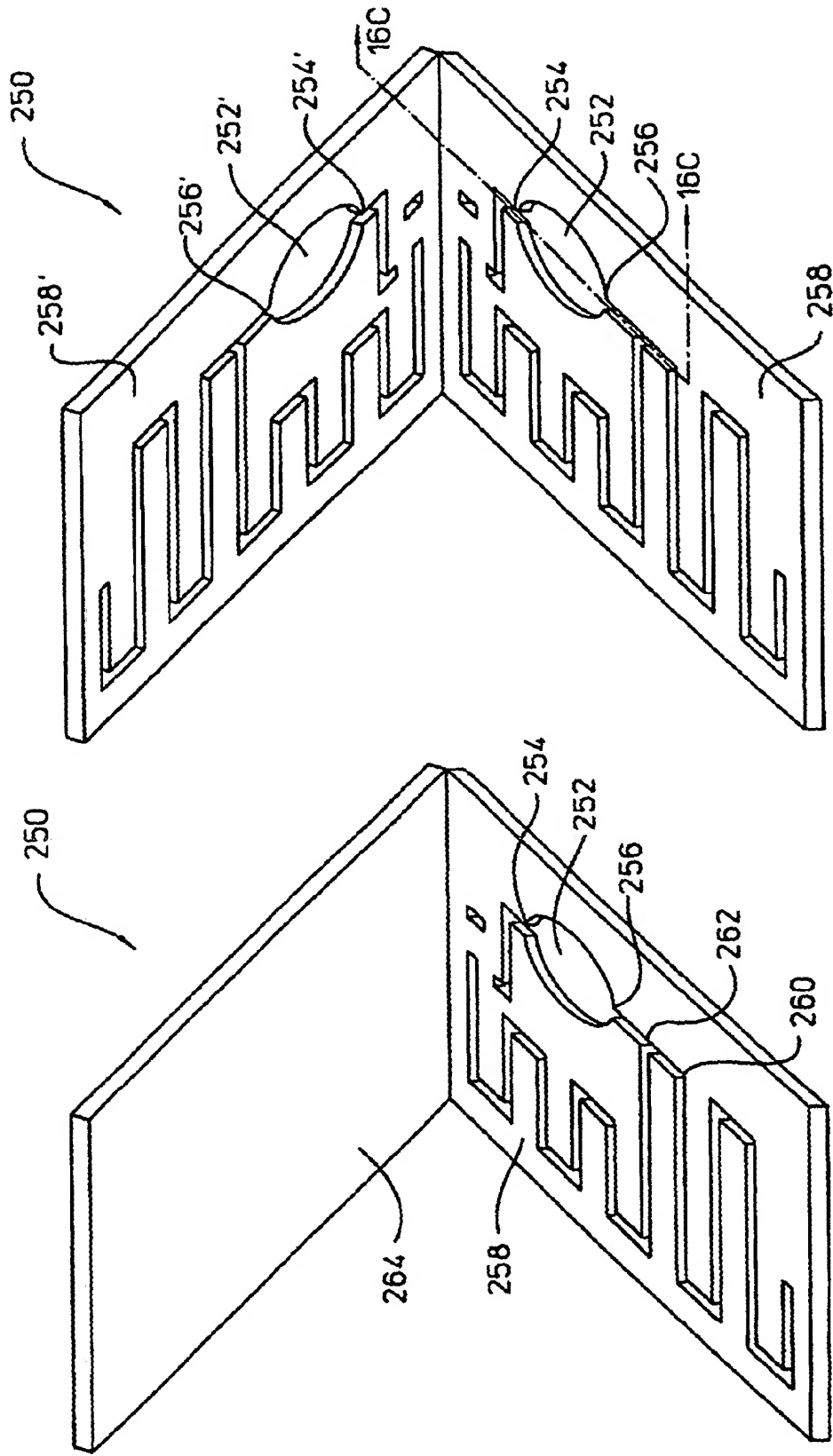


FIG. 16B

FIG. 16A

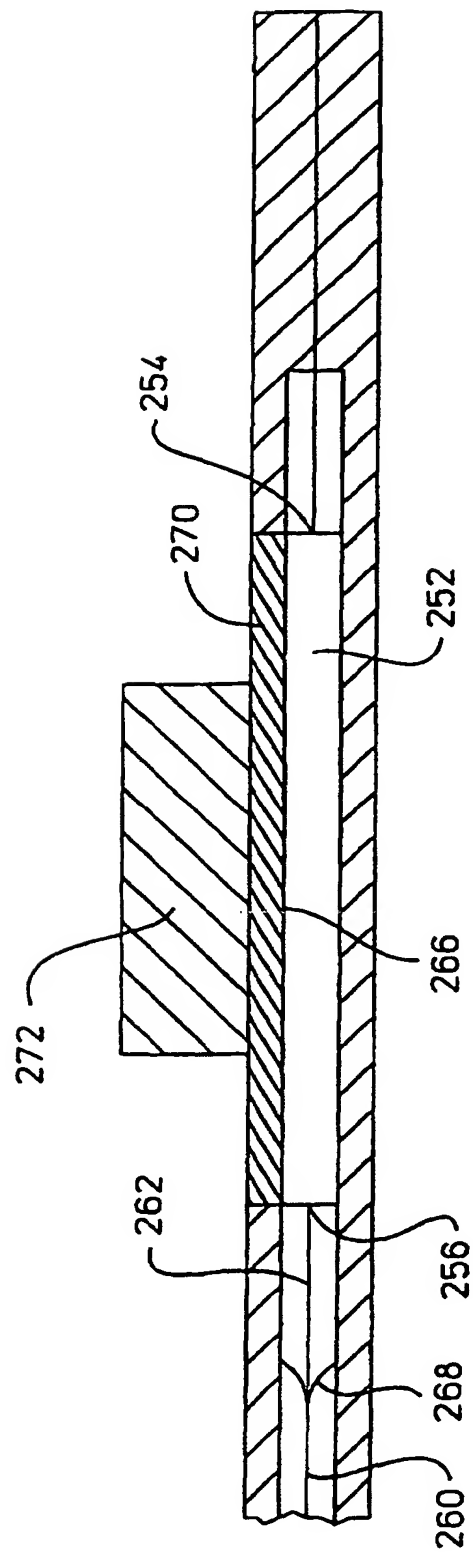


FIG. 16C

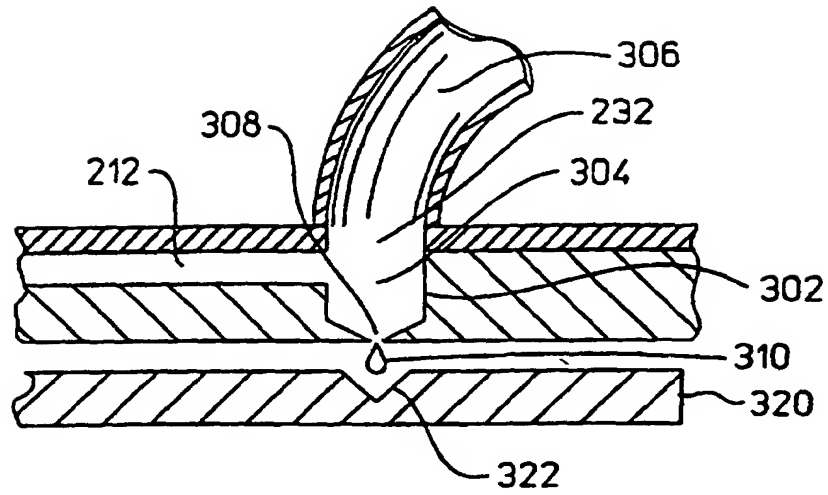


FIG. 17A

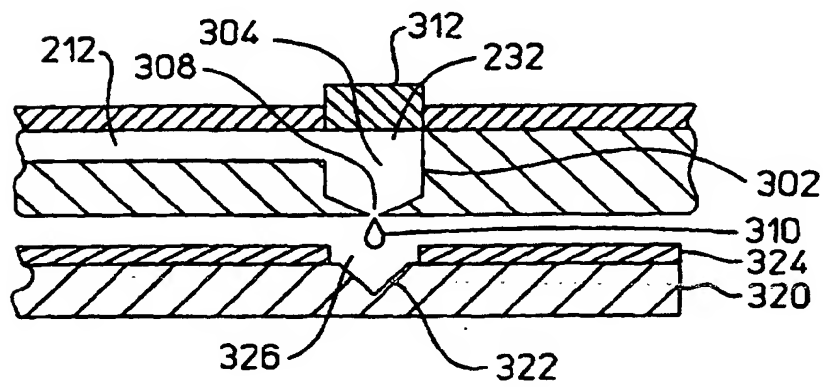


FIG. 17B

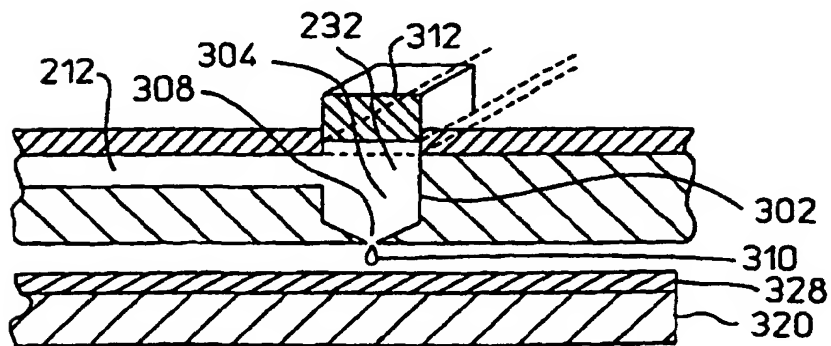


FIG. 17C

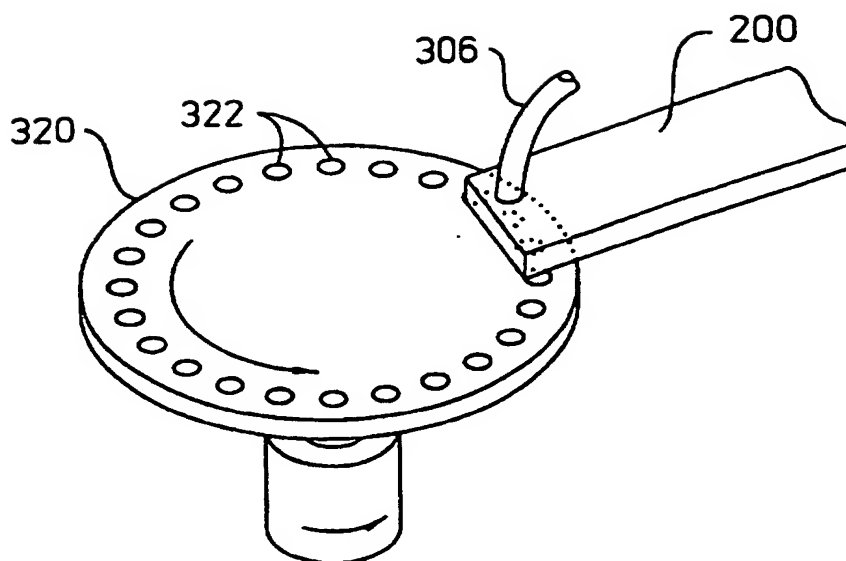


FIG. 18A

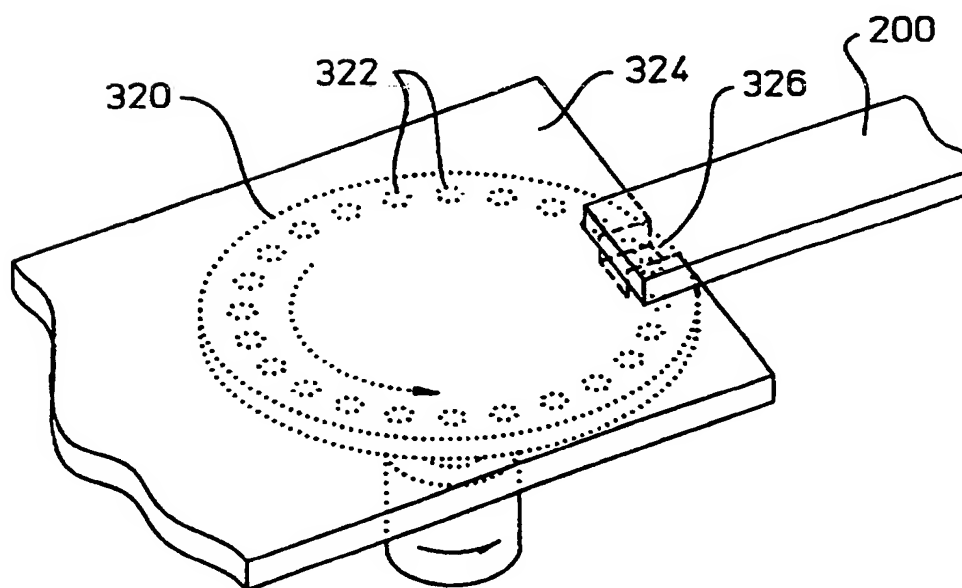


FIG. 18B